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Occupational Radiological Protection in Brachytherapy

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OCCUPATIONAL RADIOLOGICAL PROTECTION IN BRACHYTHERAPY

ICRP PUBLICATION 1XX

Approved by the Commission in Month 20XX

Abstract- Brachytherapy procedures account for an important share of occupational radiation exposure in medicine for some facilities. Additionally, staff¹ in brachytherapy treatment facilities can receive high radiation doses if radiological protection tools are not used properly. The Commission has provided recommendations for aspects of radiological protection during brachytherapy in Publications 97 (ICRP, 2005a) and 98 (ICRP, 2005b), and for training in radiological protection associated with diagnostic and interventional procedures in Publication 113 (ICRP, 2009). This report is focused specifically on occupational exposure during brachytherapy, and brings together information relevant to brachytherapy and occupational safety from the Commission's published documents. The material and recommendations in the current document have been updated to reflect the most recent recommendations of the Commission. While external beam radiation therapy results in minimal (or no) occupational doses with an appropriately shielded facility, brachytherapy uniquely presents the possibility for doses received by the staff that require active management. In modern brachytherapy centres radiation doses are incurred by staff (e.g. loading of seeds, plaques, caesium implants, associated fluoroscopy). There also exists a large variation in the practice of brachytherapy on a global scale and several facilities still practice older techniques with significantly higher staff dose potential (e.g. radium use, iridium wires). In addition, technological developments and newer techniques present new staff protection concerns that need to be addressed with specific recommendations for the practising medical community. This publication includes discussions of the biological effects of radiation, principles of radiological protection, protection of staff during brachytherapy procedures, radiological protection training and establishment of a quality assurance programme. Specific recommendations include training, monitoring and robust quality assurance programmes.

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Keywords: Occupational radiological protection; Interventional procedures; Exposure monitoring; Eye lens exposure; Protective garments

¹ As indicated in the Glossary, the term 'worker' is defined by the Commission in *Publication 103* (ICRP, 2007) as 'any person who is employed, whether full time, part time or temporarily, by an employer, and who has recognised rights and duties in relation to occupational radiological protection'. In a hospital, these persons are part of the staff. The term 'staff' is preferred in this report because the intended audience is more familiar with this term.



1

MAIN POINTS

Brachytherapy treatment utilises sources of exposure that can significantly
 contribute to occupational, patient, and public exposure, and can result in
 deterministic effects if radiological protection is not properly implemented.

Protection for patients in brachytherapy treatments, including associated imaging
 guidance during brachytherapy (e.g. CT examinations and fluoroscopy), should be
 optimised consistent with achieving the desired clinical outcome. Dose reduction
 techniques should be used whenever applicable to optimise occupational and public
 exposure.

- Staff in charge of occupational protection need knowledge of general radiological protection, but also need to be familiar with the clinical practice of brachytherapy. Likewise, individuals who perform brachytherapy should be familiar with common methods to reduce dose to patients and staff. Staff must have the appropriate education, training and certifications.
- Staff in charge of occupational protection and individuals who perform
 brachytherapy have responsibilities to family members, carers, and the public to
 answer questions and help them with understanding of their radiological protection.
- Proper use of personal monitoring is necessary in brachytherapy facilities in order to assess occupational radiation exposures. It is essential that professionals wear dosimeters correctly. Dose to an individual cannot be reasonably estimated in highly variable radiation fields without having appropriate types of individual monitoring, including extremity dosimetry, present at all times of exposure.
- A quality dose-management and quality-assurance programme are critical in establishing safe practice for brachytherapy procedures. A qualified medical physicist should be accessible to all staff, and detailed emergency response procedures, roles and responsibilities, and quality-assurance programmes available for immediate implementation. Sharing information and experience on events, within the facility and in the broader medical community, is important to continually improve protection.
- 30



1. INTRODUCTION

32 (1) Brachytherapy is a technique that places sealed radioactive sources within the human body, implanted within, adjacent to, or in contact with a target tissue. Because the absorbed 33 dose (subsequently dose) falls off rapidly with increasing distance from the sources, high doses 34 may be safely delivered to a well-localised target or region over a short time period. This report 35 36 is focused specifically on brachytherapy, and brings together information relevant to brachytherapy occupational radiological protection from the Commission's published 37 documents. The material and recommendations in the current document have been updated to 38 reflect the most recent recommendations of the Commission. 39

(2) Parallel to the development of external radiotherapy, the use of radioactive sources 40 inserted directly into tumours, or simply placed in contact, was explored in the early 20th 41 Century. This technique was called 'brachy ('short' in Greek) therapy', literally 'therapy at 42 short distances' by the English-speaking world, and curiethérapie, in order to honour the 43 discoverers of radium. Marie and Pierre Curie, in France. 44

45 (3) The technique requires that the area to be treated be accessible and that the tumour or target location be geometrically limited and be of small to moderate size. Access will generally 46 involve some type of surgical intervention. The tumour will be subjected to continuous 47 irradiation to a total prescribed therapeutic dose for as long as the sources are present. 48

(4) In the first decades of the 20th Century, most treatments were performed with 49 radioactive sources inserted or in contact, temporarily, mainly using radium tubes or needles, 50 but interest in permanently implanted sources dates back to the 1910s. Radon gas, the first 51 daughter product ('emanation') of radium, was felt to offer interesting advantages [i.e. small 52 volume per unit of activity and a very short half-life (the radioactivity becoming insignificant 53 within weeks, so that it could be implanted permanently)]. Permanent implants were initially 54 55 performed using radon emanation contained in bare glass capillary pipes, about 3 mm in length and 0.3 mm in diameter. Apart from the problems linked to the production and implantation of 56 such tiny glass pipes, another problem was that most of the dose was delivered by short-range 57 beta particles (electrons), with some 'overdosage' of the tissues located at contact or close to 58 the sources. To overcome this latter problem, tiny gold-encapsulated seeds were developed, 59 with the gold casing filtering most of the electrons and also the softer x rays, resulting in a 60 much better dose distribution. 61

(5) A large number of patients, mainly presenting with gynaecological and prostatic cancers, 62 received treatment with permanently implanted so-called radon seeds (and sometimes called 63 gold seeds because of the jackets), with favourable results in some cases. Interestingly, 64 radiographs of the pelvis after implantation of radon seeds for prostate cancer, performed in the 65 1920s, look rather 'modern', and not so different from current implantation images using ¹²⁵I 66 seeds (Aronowitz, 2002). However, this technique was progressively abandoned, mainly due 67 to the complexity of managing the radium emanations and also because, at that time, most 68 tumours were diagnosed at such an advanced stage that tumour extension exceeded the 69 possibilities of cure by any type of implantation. 70

(6) It was only in the 1950s that several groups re-activated techniques of permanently 71 implanted sources, using ¹⁹⁸Au seeds (true gold seeds). The short half-life (2.7 d) of these 72 sources allowed permanent implantation. ¹⁹⁸Au seeds were used to treat a wide variety of 73 tumours, including pelvic neoplasms. However, the use of gold seeds was progressively 74 abandoned when ¹²⁵I seeds became available in the 1970s. About the same size (4 mm in length) 75 as ¹⁹⁸Au seeds, ¹²⁵I seeds offered some advantages as the half-life is longer (60 d), which was 76



considered to be an advantage for slow-growing tumours such as prostate cancer, and the lower
 energy of its photons (~28 keV compared with 420 keV for ¹⁹⁸Au) provided for better
 radiological protection.

(7) Since that time, ¹²⁵I became the standard for permanently implanted radioactive material,
only challenged, more recently in some regions, by ¹⁰³Pd, and most recently by ¹³¹Cs. Again, a
large variety of tumours were implanted with ¹²⁵I seeds. As examples, a number of patients had
their tumour bed implanted after resection of lung carcinomas, and Memorial Hospital in New
York implemented the implantation of prostate cancer as early as 1970 (Hilaris et al., 1970;
Aronowitz, 2012). ¹²⁵I seeds had also been proposed for treating brain tumours (Marchese et al., 1984).

(8) There have been no reports to date of adverse effects to medical staff, and/or the patient's
family, associated with permanent seed implantation. This shows that the technique, already
applied to a significant number of patients can be very safe.

(9) In parallel, high-dose-rate (HDR, as opposed to the conventional low-dose-rate, LDR,
 brachytherapy described in the paragraphs above) remote-afterloaded brachytherapy gained
 wide acceptance and often in association with external irradiation (ICRP, 2005a). There is now
 growing use as single treatment for early prostate cancer.

(10) While external-beam radiation therapy results in minimal (or no) occupational doses 94 95 with an appropriately shielded facility, brachytherapy uniquely presents the possibility for doses to the staff administering the treatments. In modern brachytherapy centres, radiation 96 doses are incurred by staff (e.g. loading of seeds, sources, plaques, implants, associated 97 fluoroscopy). A brachytherapy programme represents planned exposure situations that require 98 active management. These planned exposure situations include operational exposures typical 99 to such a practice (e.g. medical exposures of patients, exposures of comforters or carers, public 100 exposures from permanent implants, and occupational exposures in applications involving 101 source handling and image-guidance) as well as potential exposures that may result from 102 emergencies or actions following accidents. 103

(11) There exists large variation in the practice of brachytherapy on a global scale and
 facilities still practice older techniques with significantly higher staff dose potential (e.g.
 radium, caesium or iridium use). In addition, technological developments and newer techniques
 present new staff protection concerns that need to be addressed with specific recommendations
 for the practicing medical community.

(12) The Commission reviewed recent epidemiological evidence suggesting that there are 109 some tissue reactions, particularly those with very late manifestation, where threshold doses 110 are or might be lower than previously considered. This is the case of the lens of the eye (ICRP, 111 2011). Recent studies have shown that there is an increased incidence of radiation-related eye 112 lens opacities in some fluoroscopy users when radiological protection devices are not used 113 properly, and radiological protection principles are not followed (Vañó et al., 1998, 2010, 114 2013a; Ciraj-Bjelac et al., 2010; Rehani et al., 2011; Jacob et al., 2012). Fairly high radiation 115 doses to the hands and legs of interventionalists and hair loss in the portions of the legs not 116 shielded by a protective device have been observed (Balter, 2001). The considerable variation 117 in operator doses observed for the same type of procedure indicates that radiological protection 118 practices can be improved (Kim and Miller, 2009). 119

(13) Physicians involved in brachytherapy procedures vary in their level of training in radiological protection. For example, in many countries, all radiologists receive training in radiation physics, radiation biology and radiological protection as part of the radiology education, but physicians in other medical disciplines receive variable amounts of education in



radiation-related topics, and may or may not be examined in these areas as part of the certification process. *Publication 113* (ICRP, 2009) provides advice and recommendations on minimum education and training, the professionals to be trained, objectives, contents, management approaches, approximate time needed to educate and train a wide variety of health professionals, accreditation and certification.

(14) The Commission has addressed specific patient-related radiation safety aspects
associated with brachytherapy in several publications, including: *Publication 86* (ICRP, 2001)
on the prevention of radiotherapy (including brachytherapy) accidents; *Publication 97* (ICRP,
2005a) on the prevention of high-dose-rate brachytherapy accidents; *Publication 98* (ICRP,
2005b) on the radiation safety aspects of brachytherapy for prostate cancer using permanently
implanted sources; and *Publication 105* (ICRP, 2008) on overall recommendations for
radiological protection in medicine.

136 **1.1. Purpose of the report**

(15) The purpose of this publication is to provide guidance on occupational protection to
personnel involved in brachytherapy, clinicians, staff, hospital administrators, medical
physicists, radiological protection officers, and those in charge of occupational protection,
clinical applications support, personnel from supplier companies, staff from dosimetry services,
regulators, and all those having an influence on the overall safety culture of the hospital.

(16) This guidance includes tools and methods for occupational protection and exposure monitoring strategies, selection, use and testing of protective garments, development of a radiological protection programme, as well as education, training, quality management, and emergency response for the programme implementation.

(17) In brachytherapy, patients are exposed to ionising radiation from different modalities
including brachytherapy, radiography, fluoroscopy, computed tomography (CT). These
modalities differ considerably in the frequency with which they are performed, in the radiation
doses the patients receive, in the way radiation is administered to the patients, and in radiation
dose to operators and staff. Radiography, fluoroscopy, and CT are not specifically addressed
in this report, but are addressed in detail in *Publications 85*, *117*, *120* and *139* (ICRP, 2000b,
2010a, 2013a, 2018).

(18) Note that this publication does not address specific radiation therapeutic methodologies associated with brachytherapy and cannot present an exhaustive discussion of brachytherapy techniques. Refer to other available guidance for specific information on clinical techniques and considerations (e.g. ICRU, 1997, 2013; IAEA, 2002, 2005). This publication is intended to emphasise the radiological protection issues associated with brachytherapy for the staff.

(19) The guidance provided in this publication applies to all types of brachytherapy 159 treatments that can generally be characterised by implant type, duration, method of source 160 loading and dose rate. Most common brachytherapy sources emit photons; however, in a few 161 specialised situations alpha-, beta-, or neutron-emitting sources are used. Intracavitary 162 treatments employ sources placed in body cavities close to the tumour volume while interstitial 163 treatments employ sources implanted within the tumour volume. Intracavitary treatments are 164 always temporary, of short duration, while interstitial treatments may be temporary or 165 permanent. Temporary implants are inserted using either manual or remote afterloading 166 procedures. Other forms of brachytherapy treatments include surface plaque, intraluminal, 167 intraoperative, and intravascular applications where either gamma-or beta-emitting sources are 168



utilised (IAEA, 2005). Recently, unique beta- (Cohen et al., 2014; Deufel et al., 2015) and
alpha-emitting sources have become available (Arazi et al., 2007; Cooks et al., 2012).

(20) Tables 1.1-1.4 summarise brachytherapy treatments with regard to the type of implant,
 duration of implant, method of source loading and dose rate (IAEA, 2005).

(21) The ICRU Report 38 (ICRU, 1985) has defined numerical values of dose rate at the 173 dose specification point(s) as a means for characterising brachytherapy by dose rate (i.e. low, 174 medium, or high dose rate) (Table 1.4). In practice, high-dose-rate (HDR) treatments are given 175 with a substantially higher dose rate, <12 Gy h⁻¹, than that given by the other two categories. 176 177 For example, the usual dose rate employed in HDR brachytherapy units is currently about 100-300 Gy h⁻¹ (Wakabayashi et al., 1971; Arai et al., 1992; Nag et al., 1999a) or 1.6-5.0 Gy min⁻¹, 178 and some modern HDR remote afterloaders contain sources capable of delivering dose rates as 179 high as 0.12 Gy s⁻¹ at 1 cm distance in tissue. Medium-dose-rate (MDR) brachytherapy is not 180 in common use because of radiobiological complexity. In those few cases in which it has been 181 used, the treatment results have been rather poor compared with low-dose-rate (LDR) or HDR 182 treatments (IAEA, 2005). 183

(22) The biological effects of radiation have been addressed in several ICRP publications
 and are summarised in Annex A with specific references for additional information. Quantities
 and units relevant to brachytherapy procedures are summarised in Annex B.

187 Table 1.1. Common Uses of Brachytherapy.

Disease Site
Breast Cancer
Oesophageal Cancer
Gynaecological Cancer
Head and Neck Cancer
Hepatocellular Carcinoma
Intravascular for restenosis and recurrent arterial blockage
Lung Cancer
Ocular Melanoma
Prostate Cancer
Skin Cancer
Soft-Tissue Sarcomas

188 Table 1.2. Characterising brachytherapy treatments by implant type (IAEA, 2005).

Type of Implant	Description
 Intracavitary	Sources are placed into body cavities close to the tumour volume.
Interstitial	Sources are implanted surgically within the tumour volume.
Surface (mould)	Sources are placed over the tissue to be treated.
Intraluminal	Sources are placed in a lumen.
Intraoperative	Sources are implanted into the target tissue during surgery.
Intravascular	Sources are placed into small or large arteries.



190	Table 1.3.	Characterising	brachyt	herapy	treatments by	y placement	duration (IAEA, 2005).
		0	2		-				/

Type of Implant	Description			
Temporary	Dose is delivered over a short period of time (from a few minutes to a few days) and the sources are removed after the prescribed dose has been reached.			
Fractionated	Dose is delivered in a series of temporary implants over a short period of time. Fractions are delivered until the total prescribed dose has been reached.			
Permanent	Dose is delivered over the lifetime of the source until complete decay.			
able 1.4. Characterising	g brachytherapy treatments by method of source loading.			
Method of Loading	Description			
Hot Loading	The applicator contains radioactive sources at the time of placement into the patient.			
Afterloading	The applicator is placed first into the target position and the radioactive sources are loaded later, either by hand (manual afterloading) or by a machine (automatic remote afterloading).			
able 1.5. Characterising	g brachytherapy treatments by dose rate (ICRU, 1985).			
Dose rate	Numerical value of the dose rate			
	at the dose specification point(s)			
Low Dose Rate (I	LDR) $0.4-2 \text{ Gy h}^{-1}$			
Medium Dose Rate	(MDR) $2-12 \text{ Gy } \text{h}^{-1}$			



2. THE ISSUES

2.1. Brachytherapy procedures 195

2.1.1. Practical source considerations 196

(23) Brachytherapy sources are usually encapsulated which serves to contain the 197 radioactivity, to provide source rigidity, and to absorb any alpha- and, for photon-emitting 198 sources, beta radiation produced through source decay. Some brachytherapy techniques (e.g. 199 ³²P plaques or films) are not encapsulated with metal or plastic, but are lightly coated with a 200 siliconised epoxy (Cohen et al., 2014; Deufel et al., 2015), and others rely on alpha-emitting 201 atoms ejected via backscattering from wires loaded with ²²⁴Ra (Arazi et al., 2007; Cooks et al., 202 203 2012).

(24) The clinically useful radiation fluence from a brachytherapy source generally consists 204 of photons, or beta particles, which can form the therapeutic component of the emitted radiation, 205 206 as well as characteristic x rays and bremsstrahlung emitted incidentally that originate in the source or capsule. 207

(25) The choice of appropriate radionuclide for a specific brachytherapy treatment depends 208 on several relevant physical and dosimetric characteristics, including: energies and penetration 209 into tissue and shielding materials, half-life, half-value layer (HVL) in shielding material, 210 specific activity, source strength. Regardless of the source used, brachytherapy is characterised 211 by the typical steep fall-off of dose with distance from the source. 212

(26) The source energy influences penetration into tissue as well as the radiological 213 protection requirements. Dose distributions in tissue, within the short treatment distances of 214 interest in brachytherapy, are not influenced significantly by photon scattering when photon 215 energies are above 300 keV. However, tissue attenuation is highly significant for low photon 216 energies of the order of 30 keV and below (IAEA, 2005). 217

(27) The shielding required to protect against high-energy photons is many 10s of 218 millimetres of lead. For low-energy photons, the required thickness is much smaller, typically 219 less than 0.1 mm of lead. 220

2.1.2. Physical source characteristics 221

(28) While the use of ²²⁶Ra and ²²²Rn was generally discontinued because of safety concern, 222 their long history of clinical use still influences modern brachytherapy concepts. Well over a 223 dozen radioactive nuclides have a history of use in brachytherapy. Some physical 224 characteristics of several brachytherapy sources are listed in Table 2.1. Table 2.2 lists 225 radionuclides most commonly used for sealed source brachytherapy procedures. 226

(29) Several available guidance documents and publications discuss specification of source 227 strength for photon emitters and the determination of absorbed dose in patients and should be 228 consulted for clinical applications of brachytherapy (e.g. ICRU, 1997). 229



Isotope	Average ¹ photon energy (MeV)	Half-life	HVL in lead (mm)	$\Gamma_{AKR}^{2,3}$ (µGy·m ²)/(GBq·h)	Dose Rate Constant ³ $(cGy \cdot h^{-1})/(cGy \cdot cm^{2} \cdot h^{-1})$
⁶⁰ Co	1.25	5.26 y	11	309	1.11
¹³⁷ Cs	0.66	30 y	6.5	77.3	1.11
¹⁹⁸ Au	0.41	2.7 d	2.5	56.2	1.13
¹⁹² Ir	0.38	73.8 d	3	108	1.12
¹²⁵ I	0.028	60 d	0.02	-	-
¹⁰³ Pd	0.021	17 d	0.01	-	-

231	Table 2.1. Physical	characteristics of several	l isotopes used in l	brachytherapy	(IAEA, 2005).
	2		1	2 12	· · · · · · · · · · · · · · · · · · ·

¹These are only approximate values, depending on the source make and filtration.

233 ² Γ_{AKR} is the air kerma rate constant.

²³⁴ ³ Using generic values of air kerma rate constant or dose rate constant for a low energy photon source may lead

to substantial errors in dose calculations. They are therefore not given here for 125 I and 103 Pd.

236	Table 2.2. Radionuclides	typically used	for implantatio	n (NCRP, 2006).
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Technique	Traditional	Current
Low dose rate	²²⁶ Ra	¹³⁷ Cs, ¹⁹² Ir
High dose rate	⁶⁰ Co	⁶⁰ Co, ¹⁹² Ir
Loaded	²²⁶ Ra	¹³⁷ Cs
Low-dose-rate Afterloaded	-	¹⁹² Ir
High-dose rate Afterloaded	-	¹⁹² Ir
Conventional-dose- rate	²²² Rn	¹⁹⁸ Au
Ultra-low-dose-rate	-	¹²⁵ I, ¹⁰³ Pd, ¹³¹ Cs
Selective internal		
Radiation therapy	-	⁹⁰ Y microspheres

237 2.1.3. Mechanical source characteristics

(30) Brachytherapy sources are available seeds or plaques. Fig. 2.1 displays severalmechanical forms.

(31) ¹⁹²Ir was historically available in the form of wires, the radioactive core being an
 iridium-platinum alloy with an outer sheath of 0.1 mm thick platinum. LDR ¹⁹²Ir sources are
 now available as seeds in strands of nylon ribbon. HDR remote-afterloading units use specially
 designed ¹⁹²Ir seed-like sources with typical initial activities of about 370 GBq.

(32) ¹²⁵I, ¹⁰³Pd, ¹³¹Cs and ¹⁹⁸Au sources are available as seeds (e.g. individual, cartridge, or
 stranded). They are usually inserted into the tumour volume using special delivery applicators.



 60 Co brachytherapy sources are available for HDR units with a typical initial activity 246 of 80 GBq. 247

(34) ⁹⁰Sr plated to the end of a rod to treat the benign disease pterygium (a non-cancerous 248 growth over the conjunctiva of the eye) using the beta radiation from the daughter product 90 Y. 249 (35) ³²P plaques are planar sources where ³²P is embedded in an epoxy polymer coated 250 with silicone.

251

(36) Novel devices have been recently developed (Arazi et al., 2007) consisting of needle 252 applicators loaded with wires to which atoms of ²²⁴Ra are securely fixated. ²²⁰Rn is emitted 253

from the wire through the decay by the alpha-emission from ²²⁴Ra. ²²⁰Rn and its progeny defuse 254

- through the surrounding tissue and deliver alpha radiation up to a few millimetres from the 255
- source. 256



257 258 Fig. 2.1. Mechanical source characteristics (ICRU, 1997).

AL is the active length. EL is the equivalent active length. PL is the physical length. S is the separation 259 between small sources. 260

2.1.4. Interventions for selective internal radiation therapy (SIRT) 261

(37) Less than 20% of patients with primary or metastatic liver cancers are curable at 262 presentation. Therefore, palliative therapies such as interventional procedures for 263 radioembolisation with the pure β-emitter ⁹⁰Y-labeled microspheres and other loco-regional 264 therapies have become alternative methods to treat patients with unresectable liver tumours 265 (Camacho et al., 2015). After catheterisation of the hepatic arteries, yttrium-90 microspheres 266 are delivered under fluoroscopic control. The rationale for SIRT is the dominant hepatic arterial 267 supply of malignant lesions while the normal liver is mostly supplied by the portal vein. Some 268 authors have suggested significant efficacy with SIRT (Bester, 2012). 269



270 **2.2. Occupational exposure**

271 2.2.1. Effective doses

(38) Annual effective doses incurred by staff depend on their function and role in the brachytherapy team (oncologists, radiographers, nurses, anaesthesia providers, medical physicists, etc.), the type of brachytherapy procedure, the medical specifics and complexity of the cases, the patient population (e.g. paediatric patients, obese patients) and other factors, such as the skill of the team, available equipment and relative use of associated imaging. Specific guidance with regard to monitoring is provided in Section 4.

(39) Summaries and compilations of data on occupational exposure associated with
concomitant fluoroscopy and interventional procedures are included in *Publication 139* (ICRP,
2018) and also available in the literature (Kim et al., 2008, 2012; ICRP, 2010a; NCRP, 2010).

281 **2.2.2.** Equivalent dose to the lens of the eye

(40) The Commission issued a Statement in 2011 published as part of *Publication 118* 282 (ICRP, 2012) after reviewing epidemiological evidence suggesting that there are some tissue 283 reactions, particularly those with very late manifestation, where threshold doses are or might 284 be lower than previously considered. For the lens of the eye, the threshold in dose is now 285 considered to be 0.5 Gy. For occupational exposure in planned exposure situations the 286 Commission now recommends an equivalent dose limit for the lens of the eve of 20 mSv y⁻¹, 287 averaged over defined periods of 5 years, with no single year exceeding 50 mSv. Although eye 288 lens dose is not typically of special concern over whole-body doses for general brachytherapy, 289 some consideration should be given with regard to the use of fluoroscopy in brachytherapy 290 procedures. Without protective eyewear, the lens dose may become the operationally restrictive 291 dose for those cases with a high volume of associated fluoroscopy imaging (Lie et al., 2008; 292 Korir et al., 2012) and the revised dose limit may be exceeded. See Publication 139 (ICRP, 293 2018) for additional information on equivalent dose to the eye lenses and associated precautions. 294 295



296 297 **3. APPLICATION OF THE SYSTEM OF OCCUPATIONAL** PROTECTION TO BRACHYTHERAPY

298 **3.1.** The principles of radiological protection

299 **3.1.1. General**

(41) The Commission's System of Radiological Protection aims primarily to protect 300 human health (ICRP, 2007). Its objectives are to manage and control exposures to ionising 301 radiation so that tissue reactions (deterministic effects) are prevented, and the risks of stochastic 302 effects are reduced to the extent reasonably achievable, societal and economic factors 303 considered. To achieve these objectives, the Commission recommends three fundamental 304 principles of radiological protection: justification, optimisation of protection, and limitation of 305 individual dose (ICRP, 2007). The principles of justification and optimisation apply to all types 306 of exposure; occupational, public and medical exposure, while the principle of dose limitation 307 only applies to workers and the public, but does not apply to medical exposures of patients, 308 carers or comforters and subjects participating in biomedical research. 309

310 **3.1.2.** Justification of practices and procedures

(42) The principle of justification is that any decision that alters the radiation exposure situations should do more good than harm. This means that when introducing a new radiation source, or working to reduce an existing exposure, or to reduce the risk of potential exposure, sufficient individual or societal benefit to offset the detriment it causes should be achieved (ICRP, 2007b,c). In the context of medical exposure, the aim of justification is to do more good than harm to the patient, subsidiary account being taken of the radiation detriment from the exposure of the radiological workers and other individuals (ICRP, 2007b).

318 **3.1.3. Optimisation of protection**

319 (43) The principle of optimisation of protection means that 'the level of protection should be the best under the prevailing circumstances, maximising the margin of benefit over harm' 320 (NCRP, 1993; ICRP, 2007b,c). More specifically, this means that 'the likelihood of incurring 321 exposures, the number of people exposed, and the magnitude of their individual doses should 322 all be kept as low as reasonably achievable, taking into account economic and societal factors 323 (the ALARA principle). In the context of medical exposure from brachytherapy, optimisation 324 of protection implies keeping patient and workers' radiation dose ALARA, consistent with 325 achieving the clinical objective of the interventions. It should be applied to the design of 326 facilities that use ionising radiation; to the selection, set-up, and use of equipment; and to day-327 to-day working procedures. 328

329 **3.1.4. Dose limitation**

(44) The principle of dose limitation states that 'the total dose to any individual from
regulated sources in planned exposure situations other than medical exposure of patients should
not exceed the appropriate limits recommended by the Commission' (ICRP, 2007b,c). This
principle applies to the exposure of medical workers.



(45) For occupationally exposed workers in brachytherapy procedures, the dose limits for
 workers recommended by ICRP apply. In planned exposure situations, recommended dose
 limits for workers were established in *Publication 103* (ICRP, 2007), with an updated limit for
 the lens of the eye in the ICRP statement on tissue reactions (ICRP, 2012).

- 338 (46) The following limits apply:
- Whole body: an effective dose of 20 mSv per year, averaged over defined periods of 5 years, provided that the effective dose does not exceed 50 mSv in any single year.
- Extremities: hands and feet, an equivalent dose of 500 mSv y⁻¹.
- Skin: an equivalent dose of 500 mSv y⁻¹, averaged over 1 cm² area of skin regardless of the area exposed.
- Lens of the eye: an equivalent dose limit for the lens of the eye of 20 mSv y⁻¹, averaged over defined periods of 5 years, provided that the equivalent dose to the lens of the eye does not exceed 50 mSv in any single year.

347 **3.1.5.** Dose constraints

(47) Optimisation is aided by setting a boundary on the predicted dose in the optimisation 348 of protection (ICRP, 2007). Such a boundary is called a dose constraint in planned exposure 349 situations, and is selected for planning purposes so that it effectively assists in the optimisation 350 process taking into account the current distribution of exposures. If later it is found to have 351 been exceeded, an investigation should be conducted to understand the circumstances, and it is 352 unlikely that protection is optimised. Dose constraints are therefore lower than the pertinent 353 annual dose limit. Dose constraints are established prospectively in the process of optimisation 354 and are source related. When staff works in more than one facility, the dose limits and 355 constraints should apply to the sum of all the individual doses incurred at the facilities. Dose 356 constraints for the lens of the eye have been suggested by the International Radiation Protection 357 Association (IRPA) (IRPA, 2017). 358

359 **3.2. Investigations of abnormal doses**

360 (48) There is no need to wait until an annual dose limit or constraint has been exceeded to 361 become aware that protection was not optimised. Non-optimised protection can be detected by 362 establishing an investigation level in terms of effective or equivalent dose received in one 363 month, or the value of a related parameter, such as the reading of the over-apron collar 364 dosimeter.

365 (49) Exceeding a monthly investigation level provides an alert that protection was less than 366 optimal in that period of time and a review of existing radiological protection is needed. The 367 increase in the dosimeter reading may be due to a substantial increase in the number of 368 interventions, or in the dose per procedure, which may be due to an increase in procedure 369 complexity or to a decrease in compliance with protection measures.

(50) In the year 2000, the World Health Organization (WHO) recommended that an investigation be carried out when monthly exposure reaches 0.5 mSv for effective dose, 5 mSv for dose to the lens of the eye, or 15 mSv to the hands or extremities (WHO, 2000). Following the new annual limit of equivalent dose to the lens of the eye, the investigation levels should be lowered accordingly. An investigation level of 2 mSv month⁻¹ (ICRP, 2018), using the reading from the collar dosimeter, may be appropriate for staff involved in brachytherapy procedures.



377 (51) An investigation level in terms of a monthly dose should be such that when 378 extrapolated to a year, it would not exceed the relevant dose limit or dose constraint. In addition, 379 personal dosimeters are not always worn or are worn improperly (Padovani et al., 2011; 380 Sánchez et al., 2012). Investigation levels can be helpful in this situation, by establishing 381 minimum dose values for the over-apron and hand dosimeters, thus providing an alert for 382 possible poor compliance with procedures for wearing dosimeters.

383 3.3. Classification of areas and workplaces

(52) Publication 57 (ICRP, 1990) discusses in paragraph 129 the possible classification of 384 workers in categories with regard to the need for individual monitoring and states that 385 interventional radiologists and cardiologists are likely to fall in category A. Classification of 386 workers, however, was not supported in Publication 60 (ICRP, 1991) and paragraph 184 of 387 Publication 103 (ICRP, 2007), states that 'The Commission continues to recommend the 388 classification of areas of work rather than the classification of workers'. The assignment of 389 individual monitoring devices should, therefore, be analysed on grounds of workplace and 390 duties of the workers, their location and time of exposure within the radiation field, and the 391 shielding provided by the protection devices used. 392

393 3.4. Embryo and foetus

(53) The Commission provided advice on the management of pregnant physicians and 394 other workers in Publication 84 (ICRP, 2000a). The early part of pregnancy (before the 395 pregnancy has been declared) is covered by the normal protection of workers, which is 396 essentially the same for males and females. The first responsibility for the protection of the 397 conceptus lies with the worker herself to declare her pregnancy to her employer as soon as the 398 pregnancy is confirmed. (ICRP, 2000a). Once the pregnancy has been declared, and the 399 employer has been notified, the working conditions of a pregnant worker should be such that 400 the additional dose to the conceptus will not exceed 1 mSv during the remainder of pregnancy 401 (ICRP, 2000a). 402

(54) Unnecessary discrimination against pregnant workers needs to be avoided. The restriction on dose to the conceptus does not mean that it is necessary for pregnant workers to avoid work with radiation completely, or that they must be prevented from entering or working in designated radiation areas (ICRP, 2000a). It does imply, however, that their employer should carefully review the exposure conditions of pregnant workers. In particular, their work should be such that the probability of high accidental radiation exposure is insignificant (ICRP, 2000a).

409 (55) As an example of a professional society guideline, a Clinical Practice Guideline for 410 the occupational radiological protection of pregnant or potentially pregnant workers in 411 interventional radiology has been developed as a joint guideline of the Society for 412 Interventional Radiology and the Cardiovascular and Interventional Radiology Society of 413 Europe (Blake et al., 2006). It states that excluding pregnant workers from fluoroscopic 414 procedures solely on the basis of radiation risks to the conceptus cannot be justified on scientific 415 grounds (Blake et al., 2006; Best et al., 2011; Dauer et al., 2015).

(56) In brachytherapy procedures, although typical occupational exposures are low, some
 considerations for pregnant workers should be made. Declared pregnant workers should not be



- expected to participate in emergency response activities associated with high-dose-rate sources (including HDR or Pulse Dose Rate, PDR sources).



421

4. INDIVIDUAL MONITORING AND DOSE ASSESSMENT

422 **4.1. Individual exposure monitoring**

423 **4.1.1.** Exposure monitoring and verification of compliance with dose limits

(57) Exposure monitoring is required for demonstrating compliance with annual dose 424 limits as well as for optimisation of protection. Monitoring compliance with dose limits 425 requires assessment of effective dose and equivalent doses to the skin, lens of the eye, hands 426 and feet. Equivalent dose and effective dose cannot be measured directly in body tissues and 427 cannot be used directly as quantities in exposure monitoring. The protection system therefore 428 includes operational quantities that can be measured and from which equivalent doses and 429 effective dose can be assessed (ICRP, 2007). Operational quantities for area and individual 430 monitoring of external exposures have been defined by ICRU and those relevant for 431 brachytherapy procedures are summarised in Annex B. 432

(58) Occupational exposure rests on a series of assumptions regarding the relationship 433 between what is measured by a dosimeter and the dose received by an individual. Standards 434 include accuracy requirements and uncertainties of the dosimetry system so that these 435 assumptions hold for the relationship between operational and protection quantities. Ensuring 436 that workers correctly wear the dosimeters during all work time is the most important 437 component of this series of assumptions and relationships. No dose to an individual can be 438 estimated reasonably in highly variable radiation fields without having some type of individual 439 monitoring on the workers during all times of exposure. Auditing compliance with procedures 440 is important to verify that the workers wear the dosimeters regularly and correctly. 441

442 **4.1.2.** Exposure monitoring and optimisation of protection

(59) For prostate implantation, lower doses correlate with increased experience of the 443 brachytherapist in the use of shielding and long-handled applicators and tools (Schiefer et al., 444 2009). In most experienced centres, several hundred procedures per year can be performed 445 prior to exceeding extremity dose limits (Schiefer et al., 2009; van Haaron et al., 2011) or 446 effective dose limits (Schwartz et al., 2003). Similarly, for eye plaque procedures, hand doses 447 were found to be low, but measurable (Laube et al., 2000; Classic et al., 2012). In endovascular 448 brachytherapy utilising ¹⁹²Ir, upper limits of whole-body dose measurements were on the order 449 450 of 10 µSv per procedure (Balter et al., 2000). Though rarely utilised now, when fluoroscopy is used in brachytherapy procedures, an increase in effective and extremity dose can be expected, 451 although with proper use of radiological protection devices, tools and techniques, effective 452 doses can be maintained well below the 20 mSv y⁻¹ limit recommended by the Commission 453 (Tsapaki, 2004; ICRP, 2007, 2018; Dendy, 2008; Miller, 2010). 454

(60) In addition to monitoring personal exposure, dosimeter use helps to increase awareness about radiological protection. In the absence of formal training in radiological protection, physicians in training tend to adopt the practices of their seniors (Rehani and Ortiz-Lopez, 2005). A strict policy on the regular use of personal dosimeters should be part of any quality programme in brachytherapy. Failure to wear monitoring equipment could be a breach of the employer's procedures and/or local regulatory or legislative requirements.

(61) Verification of compliance is not typically performed by checking doses from
 individual brachytherapy procedures but by integrating the doses over many procedures carried



out during a prescribed monitoring period. The period is established by the regulator and is
usually one month. While this period is adequate for checking compliance with annual dose
limits, it may not be sufficient for optimisation of protection in specific procedures.

(62) For associated fluoroscopic imaging, actions taken to reduce patient doses will frequently translate into reduced scattered radiation levels or the times during which elevated levels exist, thus reducing worker exposure. Separate actions may also be taken that are directed specifically at the worker. The proper use of protective shielding and locating the staff in the lower dose rate areas around the sources are examples of optimisation actions, the outcome of which can be verified by individual exposure monitoring. Over time, the impact of optimisation will appear through lower occupational doses for comparable workloads and case mix.

473 **4.2.** Characteristics of individual dosimeters and their use

474 **4.2.1.** Types of dosimeters: passive and active dosimeters

(63) Dosimeters need to have adequate accuracy under a variety of exposure conditions, 475 and to be small and lightweight enough to be convenient to use and not interfere with the staff's 476 ability to execute their tasks. Passive dosimeters are typically small, lightweight and do not 477 require power. This makes them easy to incorporate into packages that do not interfere with the 478 479 staff's actions and comfort, thus being the most widely used option, particularly for demonstrating compliance with dose limits. However, the absence of an instant reading 480 capability is a disadvantage of all passive dosimeters for optimisation monitoring, especially 481 for education of the workers involved in brachytherapy. 482

(64) For monitoring of the hands, small dosimeters on rings are used due to their relative ease of fit under surgical gloves. Rings can be sized for different finger diameters; attention is required to the fact that fingers may swell during long procedures. In addition, some additional features are important such as sterilisation capability and low interference with tactile sensation in the operator's ability to manoeuvre catheters and instruments precisely. Fingertip sachets that fit over a finger have been used as an alternative to ring dosimeters.

(65) The physical construction of the dosimeter has to be compatible with the intended wearing location. Infection control is a particular concern for ring dosimeters because some ring dosimeters do not withstand a sterilisation process, and they are typically worn during procedures where infection control is essential and thus to be worn under the surgical gloves.

(66) Dosimeters worn on the body should not create sharp pressure points that cause discomfort when placed between the heavy leaded apron and the user's clothing. If whole-body dosimeters are placed near the neck atop the leaded apron or over a protective thyroid shield to assess doses to unshielded areas, they should not have any edges that could irritate the neck or chin area. All methods of attachment should be strong enough to prevent dislodging during strenuous use but not cause dislocation of protective aprons or damage to clothing in the event the dosimeter catches on a foreign object.

500 (67) Active personal dosimeters (APDs) or electronic dosimeters may be used for 501 optimisation monitoring or for special studies that require analysis of dose by procedure or 502 discern aspects of a procedure. Active dosimeters are able to provide immediate information 503 about dose rate so that rapid feedback is available to staff against which they can assess changes 504 to their behaviour that result in lower dose rates and subsequently lower accumulated doses. 505 Dose-rate information is needed if actions are desired within a procedure as it can directly lead 506 to procedural change. In addition, active dosimeters provide information on the time of each



exposure, which facilitates correlation of occupational and patient exposures and auditing ofthe wearing of the personal dosimeter during brachytherapy.

(68) Optimisation monitoring does not need to conform to the strict dose quantities 509 required for compliance monitoring. Optimisation seeks to compare relative values resulting 510 from changes in conditions, in order to evaluate effectiveness of various actions to reduce dose. 511 Electronic dosimeters are usually calibrated to assess operational quantities without taking into 512 account the non-uniform irradiation of the body during brachytherapy procedures. That is, 513 electronic dosimeters, like all dosimeters, indicate the dose at a single point and make no 514 inferences regarding effective doses or doses at some distance from the dosimeter. 515 Conceptually, there is no technical reason why multiple electronic dosimeters could not be 516 worn and the data combined to yield compliance-type dose information, but practical issues 517 have tended to limit the use of electronic dosimeters to investigatory and optimisation 518 519 monitoring.

520 **4.2.2. Dosimeter specificity**

521 (69) To generate confidence in using a measurement made externally to the body for 522 estimating doses occurring in the body, dosimetry systems have to meet standard requirements 523 for accuracy, precision and reproducibility for the operational quantity of concern. While most 524 higher energy brachytherapy sources can be adequately monitored with standard dosimeters, 525 low-energy sources (e.g. ¹²⁵I or ¹⁰³Pd), may require special considerations and low-energy 526 dosimeters (ICRP, 2005b, Appendix B), as will beta-, alpha-, or neutron-emitting sources.

527 **4.2.3.** Dosimeter reliability and simplicity

(70) The dosimetry system must be reliable and fail-safe, that is, possess a continued ability 528 for measuring the radiation field. In addition, actions required from the user should be simple 529 and efficient to execute. For electronic dosimeters, that require the user to energise the 530 dosimeter, an item needs to be included in the procedures as an aide-mémoire for staff when 531 putting on dosimeters. The fewer the actions and decisions required from the staff, the greater 532 the likelihood of compliance with monitoring. Integrating passive dosimeters such as those 533 534 containing film, thermoluminescence dosimeter (TLD), optically stimulated luminescence dosimeter (OSL), and radiophotoluminescent glass (RPL) are generally used in the 535 brachytherapy practices for compliance monitoring. 536

537 **4.2.4.** Dosimeter exchange periods

(71) Passive dosimeters provide total dose accumulated over the period of use and at the 538 end of the use period must be exchanged for new dosimeters. The exchange period should be 539 on a predetermined schedule to instil a habitual routine among staff. Generally, fluoroscopic 540 staff should be monitored for monthly periods to provide dose data with sufficient frequency 541 that unusual events can be detected, and appropriate responses implemented. Therefore, the 542 radiation sensing material, be it TLD, OSL or film, should have the sensitivity to detect the 543 minimally relevant dose over the shortest period of expected use and should retain the dose 544 545 information for the longest expected use period.

546 **4.2.5.** Approaches to detect incorrect dosimeter wear in brachytherapy procedures



(72) Problems with wearing dosimeters may involve not only high-dose readings but also 547 very low-dose readings that may suggest misuse of, or failure to wear, dosimeters. Publication 548 139 (ICRP, 2018) gives examples of incorrect use including wearing a dosimeter that was 549 intended for use under an apron over an apron, wearing a ring dosimeter on the incorrect hand, 550 or wearing a dosimeter issued to another person. Indirect approaches (e.g. area monitoring or 551 historical doses) may be useful in identifying a lack of compliance in wearing personal 552 dosimeters and in estimating occupational doses when personal dosimeters are lost or have not 553 been used. 554

4.2.6. Different scatter conditions between type-testing and calibration and real brachytherapy procedures

(73) Monitoring to assess effective dose has been attempted using a single or two dosimeters, for example, if whole-body dosimeters are calibrated and assessed without any consideration of the effects of shielding materials. Type-test standards tend to define performance evaluations under simple conditions with dosimeters being placed on a flat surface of a tissue equivalent phantom. Assurances should be requested from the supplier to verify that the measurement of the operational quantities is within expected dosimeter performance requirements and similar conditions to that of normal use.

564 **4.2.7.** Dosimeter for the lens of the eye

(74) Monitoring of the lens of the eye presents special challenges due to the difficulties in 565 placing a device to which the dosimeter can be attached near the eyes. Small dosimeters may 566 provide opportunities for locating dosimeters near the eye and under the protective lenses. Eye 567 doses can be assessed from a dosimeter placed over the leaded apron at the collar or level of 568 the neck, or another dosimeter on a strip of plastic attached to a headband such that the sensor 569 is adjacent to the temple closest to the x-ray tube. Some attempts at eye monitoring use a TLD 570 chip wrapped in an elastic band that is fitted on the head near the eye (Bilski et al., 2011). In 571 any case, dosimeters placed near the eyes must not interfere with the wearer's vision. For 572 brachytherapy procedures, assessments of lens of eye doses can be made to decide if specific 573 eye monitoring is required, especially in the case of concomitant fluoroscopic imaging use 574 (ICRP, 2018). 575

576 **4.2.8.** Identification of the dosimeter and the worker

577 (75) Individual dosimeters should have a means to let the users identify their own 578 dosimeters. A one-to-one relationship between a dosimeter and the user is indispensable if the 579 dosimeter results are to be applied to a specific individual. Means of identification, such as 580 labels, need to be easily readable to prevent someone from using another's dosimeter. A 581 suitable approach consists of racks on which dosimeters are stored when not needed and visual 582 identification on the rack and on the dosimeter.

583 **4.2.9.** Calibration of active personal dosimeters

(76) In the course of the European project ORAMED, Clairand et al. (2011) and Sánchez
 et al. (2014) tested the influence of dose rate as well as pulse frequency and duration on the
 APDs responses. With the exception of Geiger-Müller equipped APDs, which did not give any
 signal in pulsed mode, the APDs provided a response affected by the personal dose equivalent



rate, which means that they could be used in routine monitoring provided that correction factors

are introduced. Type-test procedures and calibration of APDs and area monitors should include

⁵⁹⁰ radiation fields representative of interventional procedures, including tests in pulsed mode with

high dose rates (Chiriotti et. al., 2011; Clairand et al., 2011; Sánchez et al., 2014).

592 **4.3.** Assessment of the occupational exposure

593 **4.3.1.** Assessment of effective dose

(77) In general, effective dose is assessed from the reading of a personal dosimeter 594 calibrated in terms of personal dose equivalent, Hp(10). This assessment of effective dose is 595 sufficiently accurate for radiological protection purposes provided that the dosimeter is worn 596 in a position on the body that is representative of its exposure, under the assumption of a 597 relatively uniform whole-body exposure (ICRP, 2007). For those rare cases where 598 brachytherapy is performed under fluoroscopic guidance, Publication 139 (ICRP, 2018) 599 addresses considerations of a two-dosimeter approach, algorithms for monitoring when 600 fluoroscopy is utilised and specific guidance for assessing equivalent dose to the lens of the 601 602 eye.

603 **4.3.2.** Assessment of exposure in SIRT

604 (78) A difficulty when using β -emitters for SIRT interventional procedures is the finger 605 dosimetry of the staff. TLD finger dosimeters should be worn on the index finger of the hand 606 closer to the radiation source. Due to the very small distances between the β -source and skin 607 and the concomitantly high dose gradient the dose can be underestimated. At some workplaces, 608 Rimpler and Barth (2007) measured local skin doses Hp(0,07) at the fingertips due to direct β -609 radiation of more than 100 mSv up to about 700 mSv per working day.

610 **4.3.3.** Assessment of exposure to the embryo and foetus

(79) For pregnant workers who perform or assist in brachytherapy procedures, dose to the 611 conceptus is usually estimated using a dosimeter placed on the mother's abdomen at waist level, 612 613 under her radiation protective garments (Miller et al., 2010; NCRP, 2010). This dosimeter overestimates actual conceptus dose because radiation attenuation by the mother's tissues is 614 not considered. Specific evaluations need to be made depending on the sources being used in 615 brachytherapy. For concomitant fluoroscopic imaging, the foetal dose is typically not more 616 than half of the dose recorded on the dosimeter worn by the worker (Dauer et al., 2015), due to 617 the attenuation by the mother's abdominal wall and anterior uterine wall (Trout, 1977; Faulkner 618 and Marshall, 1993; NCRP 2010). Therefore, when two dosimeters are used, if the dosimeter 619 under the protective apron shows a value for personal dose equivalent, Hp(10) of < 0.2 mSv 620 per month, the equivalent dose to the conceptus over a nine-month period would be below the 621 limit, unless significant use of high-energy photon emitters are being utilised. Dosimeters 622 should be evaluated monthly. Electronic dosimeters can be used to provide rapid access to data 623 (Balter and Lamont, 2002). 624



5. RADIOLOGICAL PROTECTION METHODS AND PROGRAMME

627 5.1. Protection of the Staff

628 5.1.1. ALARA Principle (Time, Distance, Shielding, Planning)

(80) Occupational radiological protection requires planning so as to minimise time, maximise distance and use appropriate shielding as necessary to reduce exposures. Staff radiological protection cannot be handled independently from patient protection, since they correlate in many ways. Simple measures, such as standing a little distance away from the sources or patient, and planning ahead so as to be able to carry out procedures quickly consistent with case complexity, can be very effective in reducing occupational radiation dose.

(81) For brachytherapy procedures shielding is of four types: architectural shielding, 635 portable shielding, equipment mounted shields, and personal protective devices. Architectural 636 shielding is built into the walls of the procedure room. Rolling and stationary shields that are 637 constructed of lead, steel, or leaded glass or acrylic and rest on the floor are useful for providing 638 additional shielding for both clinicians and associated staff. These are often particularly well 639 suited for use by nurses, medical physicists, and anaesthesia personnel. In some cases, personal 640 protective devices such as a lead apron, leaded glasses, a thyroid shield, and sometimes by 641 shields suspended from the ceiling can provide protection and should be evaluated for use. 642

643 **5.1.2.** Use of Adjuvant Fluoroscopic Imaging During Brachytherapy Procedures

(82) Brachytherapy procedures using adjuvant fluoroscopic imaging often require certain
staff to remain close to the patient in order to manipulate catheters, applicators, and other
devices. Other staff who provide assistance may also need to be in close proximity to the patient.
The higher dose rates around the patient in a fluoroscopy room result from radiation scattered
back from the patient.

649 (83) Guidance for associated fluoroscopic use have been provided in *Publication 139*650 (ICRP, 2018). In addition, a number of professional societies, radiological protection
651 organisations and others have issued guidelines on practices to be followed and made
652 recommendations on the use of protective devices for associated fluoroscopic imaging (Miller
653 et al., 2010; NCRP, 2010; Chambers et al., 2011; Sauren et al., 2011; Durán et al., 2013; ICRP,
654 2013a,b; Hiles et al., 2016; Kevin et al., 2017).

655 **5.2.** Protection from external exposures

656 5.2.1. Knowledge of radiation levels around a patient

657 (84) Knowledge of the distribution of radiation levels around a patient, understanding how 658 different factors influence it, and the effective use of protective devices is indispensable for all 659 staff involved in interventions (ICRP, 2009). Radiation emanating from a patient and its 660 associated occupational exposure is determined by the brachytherapy sources employed, 661 available shielding, the complexity of the procedures, the size of the patient, the modes of 662 operation available on equipment, and the skills of the operator.



663 **5.2.2.** Personal protective equipment

(85) Staff such as nurses and anaesthesia personnel who need to remain near the patient 664 may benefit from the additional protection provided by movable (rolling) shields that can be 665 positioned between them and the brachytherapy source. Shielding effectiveness depends 666 heavily on the source characteristics and activity employed and should be evaluated by medical 667 physics and radiological protection officers. Fluoroscopic aprons can provide some protection 668 from the radiation emitted by sources of ¹²⁵I, ¹⁰³Pd, ¹³¹Cs, ⁹⁰Y by itself or in combination with 669 ⁹⁰Sr, and ³²P. For higher energy emitters, fluoroscopic aprons provide minimal protection at 670 best and can actually increase the dose to the skin. 671

672 (86) The hands of brachytherapy clinicians can be close to the sources or primary x-ray 673 beam if using image guidance. For fluoroscopic guidance, if the operators' hands stray into the 674 beam transmitted through the patient, the dose rate above the patient would be typically 2 to 5 675 μ Gy s⁻¹, so a one-minute exposure would give a dose from 100 to 300 μ Gy. Lead lined gloves 676 may be considered as protection from the fluoroscopic beam but do not allow the dexterity 677 necessary for manipulating radioactive sources.

5.3. Lifecycle of radioactive source safety

(87) Radioactive sources used in brachytherapy require safety and control along the whole
life of the source, during production, packaging, shipping, receiving, calibration, use,
decommissioning, and decay or proper disposal as waste.

(88) The physical plant facilities required for a brachytherapy programme includes a
patient treatment room or procedure room (perhaps an operating room), imaging facilities, and
a source lab (IAEA, 2008; Papagiannis and Veselaar, 2014). For radiological protection
purposes, the rooms may need to be designated according to the magnitude of expected
exposure or potential for exposure as controlled or supervised areas (IAEA, 2006; ICRP, 2007).
Aspects of brachytherapy facility design are reviewed in the literature (IAEA, 2001, 2006,
2008; NCRP, 2006; GEC ESTRO, 2018).

(89) Access to brachytherapy sources should be limited to personnel authorised for the task 689 at hand. It is generally limited to authorised users, radiation oncology physicians, medical 690 physics staff, and radiation safety staff. The radiation safety officer should maintain the active 691 list of personnel authorised access to these sources. A brachytherapy source inventory log 692 should be maintained and should include the number and activity of sources added to storage, 693 removed from storage, the patient name and room number, the time and date removed, the 694 number and activity of the sources in storage after removal, as well as the number and activity 695 of the sources returned to storage. 696

(90) Brachytherapy sources should be shielded appropriately and stored in a locked room,
 often within a locked 'safe' or location within a controlled room. Some short-lived sources are
 stored in manufacturer's shipping containers. Rooms should be posted accordingly as radiation
 control areas.

(91) All radioactive sources transported within the institution, for example to and from a
patient's room, should be moved in either a shielded cart or the manufacturer's shipping
container under constant surveillance and control of physics or radiation oncology personnel.
The transportation container should be locked or securely latched to ensure that sources are not
released if the container is dropped or inadvertently bumped. The container should be surveyed
during commissioning to ensure adequate shielding.



(92) Radiation sources used in manual brachytherapy are the most significant source of 707 occupational radiation exposure to radiation oncology personnel (NCRP, 2006) and have the 708 potential to contribute significant doses to medical personnel and others who may spend time 709 within or adjacent to rooms that contain radiation sources or patients administered various types 710 of radiation sources. Occupational and public exposure may occur during receipt, transport and 711 preparation of sources, loading and unloading sources in brachytherapy applicators, and care 712 of patients during the course of treatment. Significant dose reduction can be achieved through 713 the use of appropriate facility design associated with sources that are being prepared, are in 714 storage, or are being administered to, or are within, hospitalised patients or outpatients. 715

(93) Facility design should consider medical and physical well-being of the patient as well
as the protection of the staff, visitors and other members of the public from actual and potential
radiation hazards.

(94) Every brachytherapy facility should have the following equipment: a storage container in the treatment room to serve as an emergency source, long-handled forceps, and a portable radiation monitor instrument and an area radiation monitor (ICRP, 2005a). If there is an alarm from a radiation monitor, procedures need to be in place to respond, and assure all activity is accounted for and stored properly.

(95) Brachytherapy treatments may require the preparation of radioactive sources (e.g. 724 selection, counting, calibrating, trimming of ribbons, loading of intracavitary source inserts, 725 etc.) and should be performed in specifically designated and designed rooms. Source 726 preparation rooms (or source lab) should include consideration of the following: an area where 727 all sealed sources can be safely stored in an orderly fashion with restricted access; a method of 728 labelling and identifying sources in a shielded location, space and facilities for receiving and 729 returning sources, calibration of sources, assessment of homogeneity, inventory, and quality 730 control testing; space and equipment for source preparation for specific patient treatments; area 731 for record storage; space for treatment aids; and space for storage of short-lived sources or 732 temporary storage of unused or spent sources. Source preparation rooms should not be shared 733 with other functions. Rooms should be posted with radiation warning signs and equipped with 734 a lock to secure the area from unauthorised entry. Work benches of sufficient strength to 735 support such shielding weight and source safes should be provided. Personnel shielding that 736 facilitates source visualisation as well as personnel protection (e.g. lead blocks with leaded 737 windows, etc.) of sufficient thickness to reduce whole-body and eye exposures should be 738 provided. Occupancy of the area should be limited to persons immediately involved in source 739 preparation. 740

(96) Source manipulation should be made using forceps or tongs and never directly by
hand. Appropriate personnel shielding, such as a cave of interlocking lead bricks or a lead Lblock shield must be provided and utilised. Wipe tests for source leakage or area contamination
need to be periodically performed and the results documented.

(97) Room layout should be carefully evaluated and planned to assist in maintaining doses
ALARA. The need for the use of interlocking lead blocks on benches or wall shielding should
be assessed part of the planning. An assessment of the protection afforded to the operator and
surrounding areas should be performed prior to initiating use. Changes to shielding should be
assessed carefully.



750 5.4. Radiological Protection Considerations in Specific Applications of 751 Brachytherapy

(98) For common, specific applications of brachytherapy, the following sub-sections will
 address radiological protection considerations and will address the following factors: facility
 design and shielding, protection considerations pre-procedure, during the procedure and post procedure, and response readiness.

756 5.4.1. Manually loaded, temporary implants

(99) Manually loaded, temporary implants (e.g. LDR) brachytherapy procedures, often 757 interstitial brachytherapy, or plaque placement, is used for various tumours, especially prostate, 758 lung, brain, eye. The sources are placed directly into or onto the tumour. Such procedures often 759 can be performed by placement of applicators first followed by loading of radioactive sources 760 761 as afterloading. In other cases, the radioactive sources are placed directly into or around the target volumes with or without applicators. The placement of applicators first helps to minimise 762 unnecessary radiation exposures to the members of the medical staff (Papagiannis and 763 Venselaar, 2014). 764

(100) The careful placement of these sources for optimal treatment outcome is evaluated
based on various planning dosimetry systems (including the Manchester system, and the Paris
system) (Thomadsen et al., 2005). Several modern systems utilise reverse dose planning to
evaluate optimised source placement for tumour dose coverage (Lessard et al., 2001; Dewitt et
al., 2005).

(101) Exposure depends on a number of factors, including the radioactive sources
 themselves, and others subject to optimisation: the number of applications/years, the number
 of staff performing procedures, rotation of nursing staff.

(102) Loaded-implant techniques expose all surgical-suite personnel to ionising radiation
 and can result in the delivery of high doses to the hands of the radiation oncologist or others
 involved in the treatment.

(103) Radiation surveys (using appropriate devices - ion chamber or Geiger-Müller (GM)
probe) should be performed prior to, during, and following brachytherapy procedures.
Immediately after implanting sources in a patient, staff should make a radiation survey of the
patient and the area of use to confirm that no sources have been misplaced or lost. The survey
should cover the entire room, trash bins, equipment, clinical staff and their protective clothing.
Nothing should be removed from the room without an appropriate survey.

(104) Following an implant brachytherapy procedure, measure and record the exposure rate
 at the bedside, at 1 m from the bedside, in the visitor's area, at the doorway, and in the
 surrounding areas. Exposure rates in adjacent uncontrolled areas must conform to the local
 requirements and regulations.

(105) The patient's chart should be marked or labelled as 'Caution Radioactive Material'
during the time the sources are associated with the patient. Doors to patient rooms should be
posted 'Caution, Radioactive Material' while the sources are present in the room.

(106) Controls on visitor locations and visit durations should be established to ensure doses
to members of the public are maintained less than 1 mSv in a year and optimised to be as low
as reasonably achievable (ALARA) (ICRP, 2007). Visitors should remain within established
visitor safe areas at all times. Time limits for visits should be noted in patient or nursing
instructions.



(107) Applicator insertion is typically performed in a separate operating or procedure room
 that supports such surgical procedures needed to evaluate the patient's condition and expose or
 access the implant site. For many of these procedures, an imaging system (e.g. radiographic,
 fluoroscopic or CT unit) is required for intraoperative examination of source placement and
 geometry.

(108) Treatment room or area facilities should be designed such that consideration is given to proximity to required ancillary rooms and equipment, functional adequacy of floor space needed for shields, occupancy of surrounding uncontrolled areas, structural integrity of the building needed to support the weight of required structural or portable shielding, and ability to control entry into the room.

804 (109) Normally, designated rooms should be used for brachytherapy procedures. All rooms 805 occupied by implanted patients or containing supplies of radioactive sources should be posted 806 as controlled or restricted areas. Adjacent rooms may be used at the discretion of the 807 radiological protection officer after surveys. The patient's room should be as far away from the 808 nursing station and heavy traffic hallways as is consistent with good medical care. Ideally, this 809 would be a corner room on top or bottom floors.

(110) During treatment, patients should be housed in a private room. The entire room
 occupied by an implanted patient should be considered a controlled area.

(111) Protection of occupationally exposed persons may be met cost effectively by grouping 812 treatment rooms together in one or two limited areas rather than using individual patient 813 treatment rooms throughout the hospital. However, in some cases the goal of providing good 814 quality medical care to implanted patients may be best provided on specific floors or areas 815 based on specialised care. For example, patients with implants of the oral cavity, tongue and 816 neck may need specialised wound care, and the need to respond quickly to clinical problems 817 may demand nursing skills typically not found in other nursing units (NCRP, 2006). It is 818 possible that the development of two or three specialised facilities may be considered in high-819 volume locations (e.g. gynaecologic oncology, otorhinolaryngology, and thoracic surgery). 820

(112) Placing rooms in the corner of a building often avoids the need to shield all walls in
the designated room, especially when treatment rooms are not located at street level. Optimally,
a dedicated suite of adjacent rooms on both sides of a blind-end corridor can be designated for
brachytherapy (NCRP, 2006). Upper and lower floor rooms may also need floor or ceiling
shielding, or avoiding their occupation by 'sensitive' patients (e.g. pregnant women, children).

(113) Placing brachytherapy patients in existing, unshielded hospital rooms may expose 826 persons in adjacent areas to an effective dose that could exceed 1 mSv during the treatment 827 period. There may be specific local regulatory requirements for limiting the dose in unrestricted 828 areas that needs to be met. Several actions can be taken to minimise radiation exposure to 829 persons in adjacent areas, such as evacuation of adjacent patient rooms and use of portable 830 shielding. Radiation measurements should be made after each unshielded hospital implant to 831 confirm that the potential dose meets requirements. The radiological protection officer should 832 be consulted to determine whether adjacent rooms should be vacated or whether use of portable 833 shielding or other actions could reduce radiation exposures in adjacent areas to acceptable 834 levels (NCRP, 2006). This use of unshielded rooms should be discouraged or only accepted in 835 case of emergency (peak in occupancy). 836

(114) An intercom or video monitoring system may be useful to avoid unnecessary time
spent near an implanted patient and in reducing staff exposure (Papagiannis and Venselaar,
2014).



(115) Any patient who has received a temporary implant should not be released from under hospital care until both a radiation survey of the patient and room, and a count of the implanted sources, trains, or ribbons confirms that all sources have been removed from the patient and have been accounted. This check should be performed immediately after the removal of the sources. A record confirming the source count and radiation survey should be maintained.

(116) In some cases, high specific-activity ¹²⁵I seeds are used for temporary interstitial
implants (e.g. ophthalmological treatments). Because of the low-energy photons emitted by ¹²⁵I,
a thin lead-foil shield, a metallic applicator or even tissue overlying the implant site reduces
ambient exposure rates dramatically, eliminating or reducing potential radiation hazards to the
attending hospital staff or members of the public.

(117) Some techniques rely on balloon applicators for the treatment of malignant resection 850 cavity margins. One of the treatment options for some brain tumours, particularly gliomas, has 851 been external radiation therapy with or without the additional implantation of ¹²⁵I seeds. An 852 alternative balloon technique relies on the installation of an organically-based liquid labelled 853 with activities up to 18.5 GBq of ¹²⁵I into a balloon previously placed in the surgical cavity at 854 the time the tumour was excised (Dempsey et al, 1998). The organic liquid and the balloon are 855 then withdrawn after several days of treatment. The radiological protection considerations for 856 this treatment are more typical of radiopharmaceutical therapy and include contamination 857 concerns and radioactive waste disposal. Another consideration is the possibility of 858 radioiodinated molecules leaking out of a ruptured balloon or diffusing through the balloon 859 membrane into the cavity and being de-iodinated to liberate radioiodide which is then 860 transported to and concentrated in the thyroid (DeGuzman et al., 2003; Strzelczk and Safadi, 861 2004). Some of the solution that defuses through the balloon membrane passes into the patient's 862 urine and result in contamination (Adkinson et al., 2008). 863

(118) The treatment room or patient's room should be posted with signs, 'caution
radioactive materials' and 'radiation area', or similar. Information for visitors should be posted
at the entrance as well. The exposure rate, air kerma rate, or dose rate should be determined at
a standard distance (e.g. 1 m, 30 cm, 'contact') from the centre of the implant in the patient
with an appropriately calibrated survey meter, such as a portable ion chamber.

(119) The total exposures to medical personnel or any unsupervised individuals, including
 visitors, over the life of the implant should be assessed for consistency with the facility's
 ALARA programme. Any additional special precautions should be written down and included
 in the patient's chart as required to satisfy dose constraints and limits.

(120) Access to brachytherapy treatment rooms by healthcare personnel not involved in the treatment (or by the public) should be controlled. Typically, nursing personnel are responsible for ensuring compliance with restrictions defined in the patient's chart (NCRP, 2006). Nurses should notify a medical physicist or medical health physicist and radiation oncologist in the event of missing or displaced sources, significant changes in implant position, or any other circumstances threatening safety.

(121) A shielding container, of sufficient size and shielding effectiveness to safely hold any
sources that could become dislodged, and tools for the remote handling of a source, source train,
or applicator containing sources should remain in the patient's room for the duration of the
implant.

(122) Linens, food, utensils, rubbish and excreta should not become contaminated; however,
 linens and trash should remain in the room until surveyed to ensure that no displaced sources
 are present.



(123) During source removal, surgical dressings near the implanted applicators or sources 886 should be removed carefully and checked by an appropriately trained medical staff member 887 taking care not to dislodge the implant. Sources should be removed using a remote handling 888 device and placed immediately into a shielded container. Source inventory must be maintained 889 to verify that all sources documented on the written prescription or order have been removed 890 (visual inspection of source integrity and number). A second source-by-source (seed-by-seed) 891 count should be performed in the source preparation area. Permanent storage locations should 892 be adequate to provide both safeguarded inventory control and shielding. If at any time, a 893 source appears to be lost, the radiation oncologist, medical physicist and radiological protection 894 officer should be contacted immediately, and the rooms secured. 895

(124) Following verified removal of the sources from the patient's room, a careful survey
of the patient, the treatment room, and removed applicators should be performed using an
appropriate survey meter (e.g. a GM detector) and the results documented.

(125) Treatment rooms should not be released for cleaning and occupancy by another patient
 until the sources are securely removed, source inventory is reconciled, and the radiation survey
 verifies that no source remains in the room.

902 5.4.2. High Dose Rate and Pulsed Dose Rate

(126) Radiation exposure to hospital staff responsible for source loading and the care of 903 implant patients during treatment can be greatly reduced or eliminated by use of remote 904 afterloading technology (Glasgow, 1995; Papagiannis and Venselaar, 2014). Several robotic 905 remote afterloading systems have been developed to help minimise the radiation exposure to 906 the medical and support staff associated with afterloading techniques. In addition, the use of 907 remote afterloading devices offers several practical advantages over manual procedures, 908 including increased patient treatment capacity, and consistent and reproducible treatment 909 delivery. Such remote afterloading devices are used in both interstitial and intracavitary clinical 910 911 applications.

(127) The most common indications for HDR brachytherapy are treatment of cervical,
endometrial, oesophageal, breast, prostate, and lung cancers, skin, and soft tissue sarcomas in
adults and children. Intra-operative HDR brachytherapy is practiced in some larger facilities.

915 (128) Specific activity is an important source-selection criterion for HDR brachytherapy. The three commonly used radioactive sources in remote afterloading devices are ⁶⁰Co, ¹⁹²Ir, 916 and formerly ¹³⁷Cs (IAEA, 2005). Currently the most commonly used source for afterloading 917 918 is ¹⁹²Ir, because of its medium average photon energy (~400 keV) and its high specific activity. 919 However, its relatively short half-life is a distinct disadvantage, since frequent replacement of sources is required (typically 3 to 4 times per year) (ICRP, 2005a), involving an ongoing use 920 921 of resources and cost. Therefore, several facilities in certain countries are now employing ⁶⁰Co sources with a longer half-life. 922

(129) Most HDR systems use a single source of 192 Ir, with a typical activity of about 370-500 GBq, delivering treatment dose rates at 1 cm exceeding 4 Gy min⁻¹ (possibly as high as 8 Gy min⁻¹). A single source, (0.6-1.1 mm in diameter and 4-12 mm in length is located at the end of a drive cable or wire which sequentially stops at each programmed treatment position, or 'dwell' position. This allows for technical flexibility, as each dwell position can be placed at various positions along a catheter track and each dwell-time programmed individually.

(130) Because HDR instantaneous dose rates are so large (as high as 450 Gy h⁻¹ at 1 cm),
 this modality requires a well-organised procedure, well trained technical staff, and a
 comprehensive programme for safety, QA, and emergency procedure. The need for detailed



written procedures, checklists, written communication, and personnel training is especially
critical in HDR brachytherapy. Various groups have developed comprehensive protocols for
developing and maintaining safe treatment delivery processes (Kutcher et al., 1994; Nath et al.,
1997; Kubo et al., 1998; Kaulich et al., 1999; NCRP, 2006).

(131) Within 24 h before initiating any remote afterloading treatment, the correct operation
 of the system and its ancillary safety devices should be confirmed by performing standardised
 quality-assurance tests. Remote afterloaders should only be operated according to written
 procedures and according to a written prescription or treatment plan defining the prescribed
 treatment sequence.

941 (132) HDR treatments are staffed by radiation oncology personnel, including therapists,
 942 dosimetrists, medical physicists and radiation oncologists. Personnel need to be trained
 943 adequately on the specific model of HDR remote-afterloading system used in order to avoid
 944 possible confusion leading to errors, and to identify promptly and correct any errors that may
 945 occur.

(133) HDR facilities require an HDR treatment room, which can be a dedicated room, a 946 947 linac room, or other room (e.g. CT-scanner room normally used to plan radiation treatments so called CT simulator) built with shielding sufficient for HDR use (Glasgow and Corrigan, 948 1995). Note that CT rooms most likely would need additional shielding added to the walls, and 949 possibly ceiling and floor, to accommodate an HDR unit. Access to a radiographic imaging 950 system for treatment verification and planning is useful for a broad range of treatment 951 indications. An operating room or procedure room is also required to perform insertions, such 952 as in cervix or prostate brachytherapy. 953

(134) Inventory control and risk of the loss of individual sources is low with remote-954 955 afterloading brachytherapy units. The risk of source loss is extremely small in HDR or PDR brachytherapy as there is only one source, it is housed inside the afterloader, and that is kept in 956 a locked and controlled area. However, HDR facility design should include considerations 957 regarding security of these areas as the potential for portable sources used in HDR units to be 958 stolen and placed into so-called 'dirty bombs' has caused many facilities to substantially 959 increase the level of security for these areas. In addition, a secured facility helps to prevent 960 961 inadvertent exposure of individuals tampering with the HDR unit itself. A security plan should be developed for HDR facilities that addresses keys, locks, cameras, and tamper indicators as 962 deemed necessary. Access to the operator's key for the HDR unit control console should be 963 controlled by the radiation oncology staff and restricted to a list of specified and trained 964 individuals. 965

(135) Essential components of all remote afterloading systems are a shielded compartment 966 (or safe) to house radioactive sources (single or multiple), a local or remote operating console, 967 a source control and drive mechanism, a source transfer guide tube and treatment applicators, 968 and a treatment planning computer. Remote afterloaders are equipped with a timer that 969 automatically retracts the sources when the programmed treatment time, corrected for gaps and 970 interruptions, has been administered. HDR remote afterloaders are also typically equipped with 971 972 an inert wire, mechanically identical to the wire housing the radioactive source, that is used to verify unobstructed access to the lumens before the radioactive source is deployed. 973

974 (136) Overall requirements for HDR infrastructures can be found in IAEA documents
975 (IAEA, 1998, 2001). HDR facility design should include significant engineered and
976 administrative controls such as: 1) A door interlock system that causes the source to retract
977 automatically if the treatment room is entered while the source is out of its safe. This
978 withdrawal should result from the interruption of an interlock switch located on the treatment



room door. 2) An independent radiation monitor visible at room entrance with power back-up.
3) Appropriate radiation warning signs and 'beam on' light that is activated whenever the
source is in the exposed position. 4) Systems for maintaining visual and aural contact with the
patient during treatment (e.g. television monitoring systems and two-way intercom systems).
5) A copy of the operator's manual including emergency procedures.

(137) HDR unit or facility design should include fault detection logic capable of detecting
 source retraction failure, separation of the source from its cable, and unscheduled displacement
 of the source from its programmed positions. Systems should alert users to the problem and
 prevent further treatment. Error-detection and recovery systems located on the HDR afterloader
 should be thoroughly tested before implementation and at appropriate intervals thereafter.

989 (138) Emergency procedures should be developed for quickly detecting HDR source 990 retraction failures and bringing the source under control. These procedures should include use 991 of a radiation survey meter, and tools to safely manipulate the source and removal of the 992 applicators if needed. Emergency response equipment should be present whenever the device 993 is used, including a shielded container for source placement if unable to return the source to 994 the shielded home position.

995 (139) The radiation monitoring system that is independent of the HDR unit should be 996 installed inside the HDR treatment room to monitor the room radiation levels. Systems installed 997 at the door should give both a visible and audible signal to ensure awareness. If the area monitor 998 or treatment device indicates a source retraction failure, the responsible medical staff should 999 respond immediately. Malfunctions of the afterloader or its ancillary safety systems should be 900 brought to the immediate attention of the radiation oncologist and medical physicist present for 9101 the procedure. See Section 6 for additional emergency procedure considerations.

1002 (140) Following completion of treatment, a careful survey of the patient, the treatment room, 1003 removed applicators, and the afterloading housing should be performed using a calibrated 1004 radiation detector (e.g. GM detector) to confirm complete retraction of the sources. Survey 1005 results should be documented in the patient's treatment record. Treatment rooms should not be 1006 released for cleaning and occupancy by another patient until the radiation survey is complete 1007 and is negative for an incompletely retracted source.

1008 (141) It is estimated that more than 500 HDR accidents (including one death) have been reported along the entire chain of procedures from source packing to delivery of dose (ICRP, 1009 2005a). Human error has been the prime cause of radiation events. Many accidents could have 1010 been prevented if staff had had functional monitoring equipment and paid attention to the 1011 results. Publication 97 (ICRP, 2005a) specifically addresses the prevention of such errors and 1012 represents an important aspect of overall occupational brachytherapy radiological protection. 1013 Consider participation in the IAEA Safety in Radiation Oncology (SAFRON) voluntary 1014 reporting and learning system in radiotherapy and radionuclide therapy incidents and near 1015 misses with the purpose of sharing safety-related events and safety analysis for improved safe 1016 planning and delivery of treatments. 1017

1018 (142) Although radiation exposure to personnel is almost completely eliminated (in properly 1019 shielding facilities) for HDR procedures, there are several radiological protection 1020 considerations during high-dose-rate afterloading, including the requirement for a shielding 1021 procedure suite, constant source shielding when in the retracted position, the potential for 1022 accidental high exposures and serious errors due to increased complexity (Thomadsen et al., 1023 2003) and other problems such as failure of the source to retract.

1024 (143) For HDR treatments, survey instrumentation should be selected carefully so that the 1025 instrument does not saturate in high radiation fields. If false readings in high-intensity fields



1026 could occur, an ion chamber survey meter should be used to cover the upper extreme of the
1027 exposure-rate range. Before HDR treatment, checks should be made of the functioning of
1028 radiation detectors.

(144) PDR units have a similar design as HDR, however the activity is about a tenth of that
used for HDR brachytherapy. PDR treatments are used in large implants (e.g. sarcomas, head
and neck tumours, gynaecological, etc.). The source can be stepped with the same optimisation
possible as in HDR. Treatment is over the same duration as LDR treatments, in order to mimic
favourable radiobiology. As such, the treatment requires hospitalisation of the patient during
the administration and a dedicated and appropriately shielded treatment room where a patient
can stay for up to one or more days.

(145) PDR devices use a single 37 GBq ¹⁹²Ir source and are programmed to deliver short 1036 1037 duration HDR treatment pulses, with dose rates as high as 45 Gy h⁻¹ at 1cm, usually at hourly intervals (e.g. a source steps out for about 10 min per h and then retracts), to simulate 1038 radiobiologically continuous LDR treatments. Such fractions are described as 'pulses' and the 1039 1040 interval between successive pulses, during which the source remains in it shielded safe, is the 1041 'quiescent' period. Radiological protection considerations during PDR afterloading are similar to LDR implants, because the average hourly absorbed dose rate, in Gy m² h⁻¹, and total 1042 reference air kerma, in Gy m², are unchanged. However, the use of large pulse widths for 1043 several days may make it possible to exceed 1 mSv over the treatment duration in uncontrolled 1044 areas. Therefore, before implementing a PDR brachytherapy treatment, the user should 1045 evaluate the average hourly and weekly exposures to determine that the proposed dwell-time 1046 1047 per pulse and cumulative dwell-time will not exceed the appropriate shielding design goals. Example procedures for implementing such a requirement have been published (Williamson et 1048 1049 al., 1995).

1050 (146) Several advantages of PDR brachytherapy include that the therapy emulates LDR brachytherapy radiobiologically, it allows optimisation of the dose distribution, and visitors 1051 and staff can use the time between pulses while the source is in the safe shielded position to 1052 1053 interact with the patient. A disadvantage of PDR brachytherapy is that the lack of stability of applicators over the course of treatment is similar to that for LDR therapy. A possible 1054 1055 radiological protection disadvantage of PDR brachytherapy relates to the potential radiological 1056 safety hazard of a source stuck in the patient. LDR brachytherapy typically uses low-activity sources, which allows latitude in addressing sources that become dislodged. In HDR 1057 brachytherapy, the medical physicist or other staff are present during treatment to react quickly 1058 1059 to a radiological emergency; in PDR treatments, it may be difficult to guarantee the availability of someone with sufficient training at all times. Therefore, education and continuous exercises 1060 on emergency response procedures for on-site staff are essential radiological protection 1061 1062 programme elements for PDR (ICRP, 2005a).

1063 HDR shielding considerations –

(147) HDR brachytherapy facilities require a properly shielded area that should be designed 1064 to limit the annual effective dose to members of the public, including other patients, to 1 mSv 1065 y⁻¹ as a result of brachytherapy procedures. For adjacent controlled areas, shielding should be 1066 1067 designed to control occupational exposures to the annual dose values specified by an institution's ALARA programme. For HDR brachytherapy facilities, portable shields should 1068 not be used for this purpose. The adequacy of the proposed or existing shielding design should 1069 1070 be reviewed by a qualified expert. Before implementing HDR treatments, the dose rates in 1071 surrounding areas should be measured using properly calibrated ion-chamber survey meters



(NCRP, 2005). If the results indicate that the applicable effective dose values could be exceeded,
 the facility should limit the patient treatment workload, augment the shielding, or appropriately
 limit occupancy in surrounding areas to prevent the applicable values from being exceeded.

1075 (148) Radiation shielding should be designed by a qualified expert to ensure that the 1076 required degree of protection is achieved. The qualified expert should be consulted during the 1077 early planning stages since the shielding requirements may affect the choice of location and 1078 type of construction. Qualified experts should be provided with all pertinent information 1079 regarding the radiation equipment and its use, type of construction, and occupancy of nearby 1080 areas.

(149) This section does not attempt to summarise the regulatory or licensing requirements
 of the various authorities that may have jurisdiction over such facilities. It is expected that a
 qualified expert will be fully aware of such matters and account for them in the final shielding
 designs.

1085 (150) The exposure rate from a point-radiation source (typical in brachytherapy) in free 1086 space varies inversely as the square of the distance from the source. When the radiation source 1087 is brought outside of the shielded housing (or 'safe'), the radiation field will be essentially 1088 isotropic. Therefore, there are essentially no secondary barriers since all barriers may be 1089 exposed to the source as well as to radiation scattered from the patient and objects in the 1090 treatment room.

1091 (151) The exposure time involves the total time that the source is present outside of self-1092 shielded housing.

1093 (152) The occupancy factor for an area is the average fraction of time that the maximally exposed individual is present while the sealed source is in use and outside of its self-shielded 1094 1095 housing. For example, a waiting room might be occupied at all times during the working day, 1096 but have a very-low occupancy factor since no single person is likely to spend >50 h y⁻¹ in any given waiting room (NCRP, 2005, 2006). However, for areas where personnel are continuously 1097 present in a particular area, the occupancy factor might approach one. In most cases, the 1098 1099 maximally exposed individual will normally be an employee of the facility. The occupancy 1100 factor for controlled areas is usually assigned a value of one.

(153) In calculating required shielding, workloads should be estimated conservatively (i.e. including a safety margin) and should include source exposure anticipated for QA, source calibration, and other measurements. For example, in HDR treatments, a moderately large workload might be estimated at 100 patients per year with an average between three to five treatment fractions per patient (NCRP, 2006). It is usual to assume that the workload will be evenly distributed through the year.

(154) Source types and activities should be considered carefully in the design of shielding.
Tables of half-value layers and tenth-value layers (TVL) can be useful in designing appropriate
shielding for brachytherapy treatment. For example, Table 5.1 lists relevant information for
typical HDR sources. Lead density is typically taken to be 11.36 g cm⁻³ and normal concrete
density is estimated at 2.3 g cm⁻³.



	HVL	TVL			
I	Lead thickness (mm	ı)			
⁶⁰ Co	14	40			
¹⁹² Ir	6	20			
¹⁶⁹ Yb	1.6	5.3			
Ordinary Concrete thickness (cm)					
⁶⁰ Co	8.1	21.1			
¹⁹² Ir	4.2	14.1			
¹⁶⁹ Yb	3.4	11.4			

Table 5.1. Estimated shielding parameters for ⁶⁰Co, ¹⁹²Ir and ¹⁶⁹Yb (NCRP, 1976; Delacroix, 1998;
Granero, 2006; Lymperopoulou, 2006; CNSC, 2017).

1115 (155) For a dedicated HDR treatment room, 40 to 60 cm of ordinary concrete or from 5 to 7 cm of lead would typically be required to shield uncontrolled areas, depending on the location 1116 of the source relative to the areas under consideration and the occupancy of the adjacent areas. 1117 Every wall, the ceiling, and the floor in the HDR treatment room should serve as a primary 1118 1119 barrier. When HDR units are placed within existing linear accelerator vaults, it is typical that 1120 no additional shielding is necessary. Primary-beam teletherapy shielding is usually more than adequate for HDR treatments, however, secondary scatter shields and doors may not be 1121 adequate. The influence of HDR source position on shielding efficacy should be evaluated by 1122 a qualified expert. In those cases where shielding design restricts the source to a designated 1123 location within the room, the location should be permanently marked or fixed on the floor. In 1124 addition, such a dual-use room may need to be modified to be equipped with required interlocks 1125 for HDR as well as a method to ensure that during HDR procedures, the external beam system 1126 is locked out of use. 1127

(156) Shielding of treatment rooms should be constructed so that the shielding is not compromised by joints, by openings for ducts, pipes or other objects passing through the barriers, or by conduits, service boxes, or other structural elements embedded in the shielding barriers.

1132 **5.4.3.** Permanent implants

(157) For permanent implants, minimising radiation exposure to the staff and general public has greatly influenced the choice of radionuclide. Classically, high-energy radionuclides with half-lives on the order of a few days were used. ²²²Radon gas encapsulated in gold tubing and later ¹⁹⁸Au seeds were used for permanent implants. The patient had to be confined to a controlled area until source decay reduced ambient exposures to acceptable levels. Such classical implant types delivered high doses to the radiation oncologist's hands and exposed inpatient hospital personnel to high-energy radiation.

(158) Currently, longer-lived but very-low-energy photon emitters are used for permanent
implantation (i.e. ¹²⁵I, ¹⁰³Pd, or ¹³¹Cs). A patient's own tissues or a thin lead foil are typically
sufficient to limit exposure to the radiation oncologist's hands and fingers and eliminates the
need to hospitalise patients solely for radiological protection purposes.



(159) For prostate seed implantation, a transperineal (closed) surgical procedure, with
 ultrasound, fluoroscopy, or CT guidance is typically utilised and is most often carried out as an
 outpatient one day procedure.

(160) Various types of single-seed, seed-train and stranded-seed implantation instruments can be used to implant seeds. For single-seed applications, preloaded cartridges containing from 10-15 seeds are placed in an applicator. By ejecting each seed at a controlled distance, a linear array of seeds can be implanted. Linear arrays of seeds contained within a semi-rigid absorbable suture material are also available. Source trains can be assembled by placing sources and non-radioactive spacers of various length in needles, with or without linkages, to allow for the prescribed source distribution throughout the prostate.

1154 (161) A study of staff exposures during LDR prostate implantation procedures found that 1155 staff received about 90 μ Sv whole body and 600 μ Sv extremity doses per case (Schwartz et al., 1156 2003). They found that fluoroscopy time was the predominant factor with radiation oncologists 1157 receiving approximately 8 μ Sv min⁻¹ whole body and 50 μ Sv min⁻¹ extremity dose during active 1158 fluoroscopy. Those groups using only ultrasound guidance are expected to receive less 1159 occupational dose.

(162) There are several radiological protection considerations during permanent seed implantation, including: minimising exposure to the operator's hands, inventory control, minimising large dose-delivery errors, detecting contamination or leaking seeds, and monitoring loading trays after seed handling. Many of these actions are integral elements of an overall brachytherapy quality management system (Section 5.7).

(163) Verification of the number of seeds used has proven to be a common problem with 1165 permanent implants (Stutz et al., 2003). Inventory control is essential at all points of pre-1166 treatment planning through implementation. As the implant procedure progresses, it should be 1167 possible for a member of the implant team (e.g. medical physicist, resident, or therapist) to 1168 verify independently the seed count and source activity. If there is a discrepancy in the count, 1169 radiation safety staff should be notified and rooms should be checked for any seeds that may 1170 1171 be lost. These checks may be performed using portable radiation detectors, such as GM counters or sodium-iodide [NaI(Tl)] scintillation meters. If a CT scan is performed on the 1172 1173 patient post-implant and pre-discharge, the CT scan may be used as a further verification of the 1174 seed count if a discrepancy persists.

(164) Following completion of implantation procedures, a member of the implant team should measure radiation exposure from the patient on the surface of the patient's body and at 1 m from the approximate centre of the implant. These measurements should be made using a calibrated ionisation chamber survey meter. The readings should be entered into the patient's chart and tags or labels indicating the date on which radiation precautions are no longer necessary.

(165) As permanent implants are typically performed using low-energy emitting 1181 radionuclides, the dose rates from sources and patients who have received permanent implants 1182 is typically also low (Table 5.2). No adverse effects to medical staff or the patient's family have 1183 1184 been reported for LDR permanent implants. Several investigators have reported direct measurements on dose rates from patients. Michalski has evaluated total dose to family 1185 members of 44 patients. He gave dosimeters to the patient, spouse, children, and pets, as well 1186 1187 as monitoring four rooms frequently occupied by the patient (Michalski et al., 2003). Low levels of exposure were found, for example the mean lifetime dose to a spouse was 0.1 mSv 1188 for ¹²⁵I implant. Dauer et al. (2010) evaluated the potential doses received from prostate 1189 1190 brachytherapy implant patients in the context of developing data-based instructions. After



typical implantation with ¹²⁵I, no precautions at all were required for co-workers and 1191 nonpregnant adults (even those sleeping with the patient). As an example of suggested 1192 precautions, at their median exposure rate of 5 µSv h⁻¹ at 30 cm, the authors report that the 1193 patient should avoid sleeping 'in contact' with a pregnant patient for 84 days, and avoid holding 1194 children in the lap for long periods of time (more than 1-3 h) for 42 days. Kono et al. (2011) 1195 reported on the dose received from the implanted patients. From a series of measurements at 1196 20, 50, and 100 cm, the authors concluded that the risk from the prostate brachytherapy patients 1197 to the general public is quite low. These evaluations and measurements show that the doses to 1198 1199 staff will likely remain very low, certainly lower than the occupational limits to whole body and extremity, or even the constraint levels set for comforters and carers of such patients. 1200

(166) The Commission has previously identified radiological protection recommendations
 on the release of permanent implant patients (specifically prostate brachytherapy patients) in
 Publication 98 (ICRP, 2005b) and readers are encouraged to consult that document for more
 detailed information. A patient who has received a permanent implant cannot be discharged
 until it has been determined that the patient meets local regulatory requirements for such release.

1206	Table 5.2. Direct measurements from LDR permanent implant patients (ICRP, 2005b; Dauer et al.,
1207	2010).

	#			Anterior			Late	ral
	patients			$\mu Gy h^{-1}$			μGy	h^{-1}
				average			avera	age
				(range)			(rang	ge)
		Surface	20 cm	30 cm	50 cm	100 cm	Surface	100 cm
¹²⁵ I	19	50				< 0.3	0.06	< 0.3
Smathers		(22-89)						
^{125}I	62	26.8			2.6	0.75	1.43	0.1
Leeds		(2-67)			(0.2-5.1)	(0-1.6)	(0.1-17.4)	(0-0.5)
125 I	47	115	22				0.8	
Curie		(17-350)	(4-61)				(0.2-1.5)	
¹²⁵ I	1127	29.7		5		<0.9		<0.9
MSKCC		(1-196)		(0.1-32)				
¹⁰³ Pd	19	17				< 0.3	0.19	< 0.3
Smathers		(5-49)						
¹⁰³ Pd	152	10.4		2.1		< 0.3		< 0.3
MSKCC		(1-66)		(0.02-15)				



1208 5.4.4. Intraoperative brachytherapy procedures

(167) Several institutions with large brachytherapy programmes are utilising HDR units in
shielded operating rooms for intraoperative radiation therapy. These programmes combine
surgery and radiation oncology. The tumour is exposed and a single fraction of radiation is
delivered through the open wound. These programmes are usually only available in institutions
that can commit the resources necessary to build a dedicated brachytherapy operating-room
suite. The unique radiation safety issues of such facilities and associated shielding design have
been discussed in some publications (Anderson et al., 1999; Sephton et al., 1999; NCRP, 2006).

1216 **5.4.5. Intravascular Brachytherapy**

1217 (168) The potential role of radiation in preventing restenosis after angioplastic treatment or 1218 stent placement has been studied using brachytherapy techniques. Pre-clinical and clinical 1219 investigations used catheter-based radiation sources or radioactive stents to deliver dose to the 1220 affected coronary artery vessel wall. Sources used include ¹⁹²Ir as a medium energy γ -emitting 1221 source, and ⁹⁰Sr/⁹⁰Y, ⁹⁰Y, and ³²P as β -emitting sources (Nath et al., 1999).

1222 (169) Typical intravascular dose fraction sizes range from 10 to 20 Gy at the luminal surface 1223 or external elastic lamina at a point of about 2 to 3 mm from the catheter centre for coronary 1224 arteries and as much as 5 mm from the catheter centre for peripheral arteries. ¹⁹²Ir ribbons with 1225 dose rates as high as 4,000 G m² h⁻¹ (Tierstein et al., 1997) have been used.

1226 (170) There are several radiological protection considerations during intravascular 1227 brachytherapy, including: the high level of activity needed to produce adequate dose rates 1228 carries the potential for significant personnel exposures, and catheterised patients cannot be 1229 moved to shielded vaults for treatment.

(171) An evaluation of the shielding and the dose rates in surrounding areas should be
performed for any intravascular brachytherapy. Evaluation should consider the number of
procedures possible without exceeding the permissible dose limits in surrounding areas.
Portable shielding may be needed to supplement structural shielding (Balter et al., 2000; Bohan
et al., 2000; Folkerts et al., 2002).

(172) The failure of the sealed source to retract into its housing has been identified as a
 source of abnormal incidents with intravascular brachytherapy devices (NRC, 2004), therefore
 an additional shielded container should be available in case of emergencies.

1238 **5.4.6.** Electronically generated low-energy radiation sources

(173) Electronically generated low-energy radiation sources (ELS) refer to equipment
utilising x-ray sources with a peak voltage of up to 120 kVp to deliver a therapeutic radiation
dose to clinical targets (Devlin et al., 2017). ELS devices fall into two categories, one that is a
modern version of Grenz-ray dermatological treatment units and one that serves similar to
intracavitary brachytherapy applications, using 50 kVp x rays (electronic brachytherapy).

1244 (174) The main advantage of ELS over ¹⁹²Ir HDR brachytherapy or megavoltage electrons 1245 is that the emitted and associated scatter energy is lower allowing for much less radiation 1246 shielding. All of these devices may be used with short source-to-surface collimation, or surface 1247 applicators for treatment of tumours of the skin; the electronic brachytherapy units can also be 1248 used for intracavitary treatments, such as for breast, vagina and brain. (Bhatnagar, 2013; Ouhib 1249 et al., 2015; Safigholi et al., 2015), breast (Vaidya et al., 2014; Alvarado et al., 2015).



1250 (175) The use of low-energy radiation does not mean that ELS is without risk to patients 1251 and healthcare personnel. Some intraoperative applications of ELS have been shown to result 1252 in exposure rates to operating room staff of 2 mSv h^{-1} at about 30 cm from a treated area (Mobit 1253 et al., 2015). As in all forms of radiation therapy, ELS requires proper initial and ongoing 1254 training of the entire treatment team, with detailed attention to personnel, equipment, patient, 1255 and personnel safety (Devlin et al., 2017).

(176) Techniques in risk analysis and development of a quality management programme for
electronic brachytherapy has been developed by a task group of the American Association of
Physicists in Medicine based on the principles of TG 100 (Huq et al., 2016; Thomadsen et al.,
2020).

1260 **5.4.7.** Selective internal radiation therapy (SIRT)

(177) SIRT is a technique to deliver radiotherapy treatment for cancer or metastases in the 1261 liver. SIRT is generally implemented by interventional radiology, nuclear medicine physicians 1262 and radiation oncologists. Vials containing ⁹⁰Y labelled microspheres should be handled with 1263 forceps and appropriate shielding to reduce finger doses. Due to the high-energy beta emission, 1264 shielding is best provided with a low-atomic-number material, such as polymethyl methacrylate 1265 (PMMA). Vendors of SIRT spheres provide advice and training material to minimise the 1266 contamination risk to staff, patients and the room (SIRTEX, 2016). This includes the use of 1267 special shielding boxes for preparation and injection. Furthermore, double gloves are 1268 recommended to allow removal of a contaminated outer glove with a gloved hand. For 1269 implantation of the microspheres the vendor provides an acrylic delivery box and delivery set. 1270 This prevents direct contact with the ⁹⁰Y vial and all stopcocks or tubes. Table 5.3 gives a 1271 1272 representative overview on typical exposure of the different staff members for a single SIRT procedure. The actual values depend on the type of microspheres used. ICRP has developed 1273 additional guidance associated with SIRT in Publication 140 (ICRP, 2019). 1274

		Trunk (mSv)	Lens of the eye	Hands
			(mSv)	(mSv)
Pharmacist	$H_{\rm p}(0.07)$	0.027	0.026	0.35
	$H_{\rm p}(10)$	0.003	0.004	
Interventionalist	$H_{\rm p}(0.07)$	0.038	0.12	0.32
	$H_{\rm p}(10)$	0.004	0.054	
Radiation safety	$H_{\rm p}(0.07)$	< 0.02	0.04	0.2
	$H_{\rm p}(10)$	0.01	0.017	

Table 5.3. Representative exposures for the technician or pharmacist preparing a typical patient administration, and for the physician implanting that prepared dose (SIRTEX, 2016).

1277 (178) Only a few papers on occupational doses from SIRT have been published. 1278 Occupational exposure from SIRT procedures is caused both by x rays with relatively low dose 1279 rate and by direct β radiation, especially to the hands and fingers with high dose rates if 1280 precautions are inadequate. In addition to the dose to the hands of workers preparing the 1281 individual patient dose and to the physician implanting the microspheres, there is potential for 1282 significant contamination hazard. Exposure data are 43.5 mSv MBq⁻¹ h⁻¹ skin equivalent dose



1283 due to contact with a 5-ml syringe and 1.35 mSv kBq⁻¹ h⁻¹ due to contamination with 50 μ l on 1284 1 cm² (Kemerink et al., 2012). Specific advice to reduce this hazard is given in *Publication 140* 1285 (ICRP, 2019).

(179) In addition to all technical measures of radiological protection, training to efficiently
 perform all steps of the procedure leads to a significant reduction of occupational exposure.
 Aubert et al. (2003) demonstrated extremity dose reduction by optimising the ⁹⁰Y injection
 technique. They found an extremity dose reduction factor of more than 10 after optimisation of
 the procedure.

1291 (180) After the SIRT, the patient requires observation, general nursing care, and 1292 accommodation. McCann et al. (2012) determined in 143 SIRT procedures (124 with resin 1293 spheres and 19 with glass spheres) mean equivalent dose rates of $1.1 \ \mu\text{Sv} \ h^{-1}$ at 1 m for resin 1294 spheres and 2.4 $\mu\text{Sv} \ h^{-1}$ at 1 m for glass spheres. Typical dose equivalent rates 6 hours after 1295 implant of 2 GBq ⁹⁰Y activity (SIRTEX, 2016) are shown in Table 5.4 for different distances.

Table 5.4. Typical ambient dose equivalent rates 6 hours after implant of 2 GBq ⁹⁰Y activity for different
 distances.

Distance from the sources	Ambient Dose equivalent rate
0.25 m	18.8 μSv h ⁻¹
0.5 m	9.2 μ Sv h ⁻¹
1 m	1.5 μSv h ⁻¹
2 m	0.4 µSv h ⁻¹
4 m	$<0.1 \ \mu Sv \ h^{-1}$

1298 5.5. Education, training, and credentialing

(181) The Commission has addressed the specifics of minimum levels of training for
 interventionalists, nuclear medicine specialists, medical physicists, nurses and radiographers or
 technologists, among others, in *Publication 113* (ICRP, 2009).

(182) The International Basic Safety Standards for Protection against Ionizing Radiation and
for the Safety of Radiation Sources (BSS), published by the International Atomic Energy
Agency (IAEA) and jointly sponsored by, among others, the Food and Agriculture
Organization (FAO), the International Labour Organization (ILO), the Pan American Health
Organization (PAHO) and the World Health Organization (WHO) (IAEA, 2014a), require
appropriate training that is sufficient to perform assigned tasks in the safe conduct of diagnostic
or therapeutic procedures involving radiation.

(183) Legislation in most countries requires that individuals who take responsibilities for
 medical exposure must be properly trained in radiological protection. However, a training
 system and accreditation mechanism is still lacking in some countries.

(184) *Publication 97* has provided specifications for personnel requirements and training
that are applicable for all brachytherapy facilities in general and should be consulted. Clearly,
a major prerequisite for the development of a safe brachytherapy facility is adequately trained
staff (ICRP, 2005a). A multidisciplinary team should be organised including, at a minimum, a
radiation oncologist, a medical physicist, a technician, and a nurse.



(185) All brachytherapy team members must receive adequate training (and certification
where appropriate) in the brachytherapy procedures to be implemented before being authorised
to perform (or take part in) the procedures. Training programmes should include both initial
training for all incoming staff and regular updates and retraining.

(186) Specific training in radiological protection must also be performed. Training activities 1321 should be followed by an evaluation of the knowledge acquired from the training programme 1322 to test competency before the person is awarded certification. If certification in radiation 1323 protection is required for some medical specialties, certification should be obtained before the 1324 individual is permitted to practice the specialty. Scientific and professional societies should 1325 contribute to the development of the training syllabi to ensure a consistent approach, and to 1326 1327 promote and support the education and training. Scientific congresses should include refresher courses on RP, attendance at which could be a requirement for continuing professional 1328 development for professionals who use ionising radiation (ICRP, 2009). 1329

(187) Facilities performing brachytherapy should provide oral and written radiation safety instructions to all personnel involved in patient care associated with brachytherapy. Refresher training at periodic intervals should also be provided. At a minimum, the radiation safety instructions should include information regarding the size and appearance of brachytherapy sources, safe handling and shielding instructions in the event a source becomes dislodged, as well as procedures for notifying the radiation oncologist and radiation safety officer if the patient dies or has a medical emergency.

(188) In addition to general knowledge on radiological protection, all staff participating in
brachytherapy procedures guided by radiological imaging need awareness of the distribution
of scattered radiation levels around a patient, understanding of how different factors influence
the dose distribution, and familiarity with the effective use of protective devices, such as shields,
leaded eyewear and shielding curtains and drapes. This knowledge should be achieved by initial
training and maintained and updated through continuous education, consistent with the
evolution of technology.

(189) The radiation oncologist is responsible for the overall procedure, as brachytherapy is
a medical treatment. He/she should be properly accredited according to each country's
regulations. Specific responsibilities of the radiation oncologist or interventional radiologist,
nuclear medicine physician, and surgical oncologist include (Kutcher et al., 1994):

- 1348 Patient evaluation;
- Patient selection;
- 1350 Treatment protocol selection;
- 1351 Treatment prescription
- 1352 Applicator insertion(s)
- 1353 Imaging review;
- Selecting tumour, target, and treatment volumes;
- 1355 Treatment plan approval;
- 1356 Applicator(s) removal;
- 1357 Evaluation of tumour response and side effects;
- 1358 Implementation of radiation safety instructions and emergency procedures; and
- 1359 Patient follow-up.

1360 (190) Even if the radiation oncologist has experience in either HDR or LDR brachytherapy,

additional training is required in the other type of brachytherapy (ICRP, 2005a). 'Hands-on'training is highly indispensable.



(191) The medical physicists and radiological protection specialists providing support to
brachytherapy facilities should have the highest level of training in radiological protection as
they have additional responsibilities as trainers for oncologists and other health professionals
involved in the procedures (ICRP, 2009). Specific responsibilities of the medical physicist
include, at a minimum:

- Equipment life cycle, including testing equipment at the time of acceptance of new equipment or after major repairs;
- Verification of calibration of sources;
- Performing source exchange, if necessary;
- Checking the treatment unit verifying source positioning, indexing, internal gamma alarm, etc.;
- Checking patient set-up including applicator positioning;
- 1375 Supervising imaging;
- 1376 Treatment planning and calculations;
- 1377 Implementation of radiation safety instructions and emergency procedures; and
- Supervising treatment administration by the technicians.

(192) The medical physicist should participate in preparation of the patient after the
applicator has been inserted and prior to obtaining images, since it is during such preparation
that x-ray marker wires are to be positioned in the applicators as necessary. It is also necessary
to select the angles of radiographic images or to select planes in the event of verification by CT
or MRI.

(193) For HDR treatments, the medical physicist should be trained in the use of the HDR
planning system and should become thoroughly familiar with applicator image reconstruction.
Training in equipment use, security systems, and emergency procedures are mandatory.
Medical physicists should also be trained in the basic principles and procedures of radiological
protection.

(194) Personnel monitoring services staff need background knowledge of the clinical
 practice for calibrating dosimeters appropriate for brachytherapy and any associated
 fluoroscopic use (e.g. radiation qualities, scatter radiation fields, pulsed radiation) and for
 investigating abnormal dose values.

1393 (195) Technologists and brachytherapy technologists are typically in charge of the 1394 following:

- Checking applicators and specific accessories (alternatively nurse);
- 1396 Daily checking of treatment units;
- Assisting the radiation oncologist during implantation (alternatively nurse);
- 1398 Obtaining images for localisation;
- Using treatment planning under the medical physicist's supervision;
- Delivering treatment (for HDR or LDR afterloading devices, etc.);
- 1401 Monitoring each treatment from the console;
- Implementation of radiation safety instruction and emergency procedures; and
- 1403 Recording treatment on appropriate documents.
- (196) Nurses are typically in charge of assisting the physician during each procedure.
 Specific responsibilities include:
- Daily checking of the treatment or patient rooms;
- Ensuring supplies of disposables, gynaecological packs, etc.;
- Scheduling of patients (alternatively a technologists or other clinician);
- Receiving patients and sending them home;



- Implementation of written discharge instructions that include radiation safety instructions
 and emergency procedures; and
- Assisting the radiation oncologist/interventional radiologist during implantation.

(197) The role of the manufacturers is of increasing importance (ICRP, 2010c). There is a need for the design of built-in safety engineering, careful and tested software, design of informative warnings, self-test capabilities, self-explanatory user interfaces, and internal safety interlocks to prevent improper use that may lead to accidental exposures. Technology- and technique-specific training are important for users, as well as installation and maintenance engineers.

1419 **5.6. Records related to occupational protection**

(198) The records to be kept are established as requirements in standards and regulations. 1420 Records of occupational exposure include information on the nature of the work in which the 1421 1422 worker is subject to occupational exposure monitoring; including, for interventional staff, information on work for other employers that involves radiation exposure; outcomes of health 1423 surveillance; education and training on radiological protection, including refresher courses; and 1424 results of exposure monitoring and dose assessments, including results of investigation of 1425 abnormal exposure values. Employers should provide staff with access to records of their own 1426 occupational exposure. 1427

(199) Information on workload, in terms of procedures per year, is useful for optimisationof protection and for comparing and investigating unusual exposure.

1430 5.7. Quality Management System

(200) All facilities performing brachytherapy procedures should establish a comprehensive 1431 quality-management programme with well-defined objectives to ensure compliance with 1432 standard good practices. Quality-assurance programmes (QAP) in brachytherapy should cover 1433 all of the planned and systematic actions necessary to provide confidence that optimum quality 1434 has been achieved in the entire diagnostic and treatment process. The programme should 1435 include aims for maintaining best radiological protection practice to ensure appropriate 1436 occupational exposure control (ICRP, 2007; IAEA, 2014a). Active participation of the staff 1437 involved in the use of radiation is advisable, taking into account the Commission's 1438 1439 recommendations for planned exposure situations. The programme should be part of the 1440 management system implemented at the institutional level, including regular and independent audits, internal and external. 1441

(201) A QAP for brachytherapy includes all of the aspects of radiological protection of
patients and staff in addition to the usual clinical aspects. The QA programme should include
physical, clinical, and organisational aspects applicable to the brachytherapy modality. The
details of a full clinical QA programme are beyond the scope of this report and the reader is
referred to several documents (e.g. Kubo et al., 1998; IAEA, 1998, 2001; NCRP, 2006)

1447 (202) Most clinical QAP programmes have as their main objectives: the preparation of a 1448 physician's written directive before administration of treatment, clear identification of the 1449 patients, documentation of treatment and related calculations, compliance of each treatment 1450 with the written directive, and the identification and evaluation of any unintended deviation 1451 from the prescription.



(203) A radiological protection programme must be established to ensure compliance with 1452 regulations for radiation safety and protection as promulgated by local governing agencies 1453 (IAEA, 2001, 2008). A qualified radiological protection officer, who is responsible for 1454 implementing the radiological protection programme, should be identified, officially appointed, 1455 and given sufficient administrative authority, in writing, to supervise the programme. A 1456 radiological protection committee should also be established and should include, at a minimum, 1457 an authorised user of each type of use permitted by the licence: the radiation safety officer, a 1458 representative of the nursing service, and a representative of management. 1459

(204) Two basic objectives of the radiological protection QAP are to evaluate patient
radiation dose on a periodic basis and to monitor occupational radiation dose for workers in
brachytherapy facilities where radiation is used. The radiological protection component of the
QAP for brachytherapy should be an independent portion of the general QAP for x-ray,
radiation oncology and nuclear medicine installations in a particular health centre.

(205) The Radiological Protection Advisor or Radiation Safety Officer should be involved
in monitoring occupational radiation dose. The QAP for brachytherapy should be reviewed at
least annually, to allow the opportunity for updates and periodic follow up. Self-audit of the
QAP is also advisable.

(206) The design of a new brachytherapy facility, the selection and the upgrade of existing equipment are all complex and expensive processes. Planning for these processes should include radiological protection. A senior physician, a medical physicist and a radiological protection officer should be included in this planning. Physicians representing all of the medical specialties who will be using the new room should be involved in specifying the equipment for the room.

1475 (207) The following paragraphs discuss some of the major activities required by a QAP.

(208) Source Commissioning - Wipe Tests. A package containing a shipment of radionuclide 1476 must be monitored immediately upon receipt for any physical damage or excessive radiation 1477 levels. Wipe tests for any contamination should be carried out on the package surface. 1478 1479 Radiation levels should be measured and recorded both at the surface and at 1 m distance and compared with the shipping label. Individual large encapsulated sources should be wipe tested 1480 1481 for possible leakage or contamination. This should be performed at the time of receipt of new sources and at six monthly intervals for sources with a long half-life that are kept in the 1482 permanent inventory. A source is considered to be leaking if ~200 Bq of removable 1483 contamination is measured. The measurement is usually performed using a sensitive 1484 scintillation well counter or a liquid scintillation counter. For permanent implants with seeds 1485 which are delivered sterile (usually in sterile cartridges), it is not realistic to test (dosimetry and 1486 wipe test) all the seeds to be implanted. In such cases it is recommended to test the outside of 1487 the vial containing the seeds at delivery, and the inside of the cap of the vial when the vial is 1488 1489 opened.

(209) *Calibration Chain* - Brachytherapy sources should have their source strength
calibrations traceable to a national standards laboratory. In some instances, it may be necessary
to establish a second level of traceability by comparison with the same type of calibrated source.
Guidelines for the number of sources in a sample that should be measured can be found in
Butler et al. (2006).

(210) Constancy Check of Calibrated Dosimeter - Constancy response of the calibrated
 dosimeter system may be checked by periodic measurement of a long half-life source, such as
 ¹³⁷Cs (or other acceptable source) in the case of a well type chamber. Reproducible positioning



is important. Such periodic measurements also provide a good quality assurance check of theentire measuring system.

(211) *Regular Checks of Sources and Applicators* - Mechanical integrity of a long-lived
source must be checked at regular intervals by visual inspection, leak testing and activity
measurement. Source strength and wipe tests should be performed on a periodic frequency
(such as semi-annual basis). Visual inspection and radiographic evaluation of all applicators
should be performed at some established frequency, including checks for structural soundness,
that all clamps, screws and retaining devices are functioning properly and that the source insert
carriers seat correctly.

- (212) An important aspect of the QAP is a description of the roles and responsibilities of 1507 1508 personnel. There should be enough staff to avoid an excessive number of procedures per specialist, and sufficient nursing and technologist support. Support by network specialists (for 1509 new digital systems), maintenance and service personnel and medical physics specialists is 1510 advised. Medical physicists should be active in brachytherapy departments. They should work 1511 with radiation oncologists to assure that proper equipment is purchased and utilised. Medical 1512 1513 physicists can guide radiation oncologists in achieving the proper balance capability and safety, and oversee the training of all members of the department. 1514
- 1515 (213) Procedures should be in place for new staff expected to be involved in interventions 1516 guided by radiological imaging to ensure the following: their education and training in 1517 radiological protection, arrangements for obtaining and evaluating their previous dosimetric 1518 history, pre-employment health surveillance, and arrangements for sharing information with 1519 other employers in case the staff works in more than one place.
- 1520 (214) Procedures should be in place for the selection of the appropriate radiation detectors 1521 and dosimetry equipment. Arrangements for staff radiological protection and health 1522 surveillance should be in place, with monitoring of body, eye and hand exposure as well as 1523 workplace monitoring, as set forth in the radiological protection programme. Personal 1524 protective devices, such as aprons, thyroid shields and leaded eyewear, as well as ceiling-1525 suspended shields and table-mounted curtains should be made available when appropriate.
- (215) Analysis of staff radiation dose should be included in the QAP. Calibrated dosimeters 1526 1527 for staff must be available. Personnel working in fluoroscopy laboratories should wear appropriate dosimeters, and a strict policy for their use should be implemented. Additional 1528 electronic dosimeters may also be useful, especially for radiological protection training of 1529 students and inexperienced personnel. The QAP should ensure the regular use of personal 1530 dosimeters and include a review of all abnormal dose values. Results of personal exposure 1531 monitoring and workplace monitoring should be recorded, as well as the necessary corrective 1532 measures taken in response to unusual results. Personal dosimetry suppliers should document 1533 the accreditation and performance in dose assessment from the supplied personal dosimeters 1534 and the information be recorded and kept safe for regulatory recommended time. Procedures 1535 should include investigation, reporting and recording results and audits of occupational doses 1536 as well as corrective actions in case of incidents or accident. 1537
- (216) It is extremely important that there be immediate local reporting and analysis of all accidental exposure of staff as well as unexpected events. This should be followed by the identification of causes, contributing factors, and extent of conditions; all of which should result in corrective measures. Responses to such situations should be followed by rapid and widespread circulation of the relevant information, to avoid similar problems being reproduced in another centre. Institutions should consider participation in the IAEA Safety in Radiation Oncology (SAFRON) voluntary reporting and learning system in radiotherapy and



radionuclide therapy incidents and near misses with the purpose of sharing safety-related eventsand safety analysis for improved safe planning and delivery of treatments.

(217) Procedures should address the requirement and instructions for wearing protective
devices to the extent possible and compatible with the success of the interventions, including
the use of ceiling-suspended shields and protective eyewear. Procedures should also include
audits and recording of the wearing of protective eyewear, especially if a dose reduction factor
is applied to dosimeter readings to account for the attenuation.

(218) Radiological protection training and certification of brachytherapy and interventional staff should be documented and subject to reviews at established periods or whenever there is a significant change. Induction training in the operation of the quality assurance system should be part of the strategy of the organisation. Administrative procedures including the assignment of responsibility for quality assurance actions and for reviewing and assessing the overall effectiveness of radiological protection measures need to be established and be part of the quality assurance manual.

1559 (219) For fluoroscopy and CT systems, acceptance tests should be made by the company 1560 supplying the equipment in the presence of technical personnel from the centre buying the 1561 system, or by centre technical personnel. This should include tests to determine the 1562 functionality of the radiation safety features of the equipment. Commissioning of the new 1563 equipment before its clinical use should be the responsibility of the personnel of the centre.

1564 (220) Periodic quality control (QC), including dosimeter calibration, should be planned, 1565 taking into account international standards, local regulatory requirements, local 1566 recommendations and the recommendations of the x-ray system manufacturer. These should 1567 also include practical results, to assist the radiation oncologist in appropriate management of 1568 patient doses (e.g. dose rate in different fluoroscopy modes, CT scan protocols).

(221) For fluoroscopy and CT systems, periodic evaluation of image quality and procedure 1569 protocols should also be included in the QAP. Image quality should be measured with test 1570 objects during the acceptance and constancy tests. With digital imaging detectors, it is possible 1571 1572 to select a wide range of dose values to obtain the required level of quality in the images. It is easy to specify excessive dose rates, as these do not impair image quality and are not easily 1573 1574 detected from inspection of the image. Radiation oncologists, in cooperation with 1575 radiographers/technologists, the medical physicist and the industry engineer should set the fluoroscopic or CT system doses to achieve the appropriate balance between image quality and 1576 dose needed during brachytherapy planning, treatment, and follow-up. 1577

1578 (222) For each imaging modality they use, radiation oncologists should learn the dose 1579 required to obtain an adequate level of diagnostic information.

(223) Since occupational protection is closely related to patient protection, the overall
 quality assurance programme should include quality control of the radiological equipment,
 acceptance testing and commissioning, full characterisation of the radiological equipment, the
 calibration of the air kerma area product (PKA) meters, as well as quality control of the personal
 protective devices.



1586 6. EMERGENCY PLAN AND RESPONSE IN BRACHYTHERAPY

1587 6.1. Need for Emergency Plans and Response Readiness

(224) Accidents associated with brachytherapy procedures have been reported and some of them have had significant impacts on staff safety, especially those involving HDR brachytherapy (ICRP, 2005a). Indeed, more than 500 HDR brachytherapy accidents (including one death) have been reported along the entire chain of procedures from source packing to delivery of dose. Human error has been the prime cause of radiation events. Many accidents could have been prevented if staff had had functional monitoring equipment, paid attention to the results, and responded quickly and appropriately.

- 1595 (225) Such events have different origins (ICRP, 2005a), including:
- 1596 Incorrect measurements leading to erroneous source positioning;
- 1597 The handling and transport of the sources;
- 1598 Inadequate shielding;
- Sources in transit (sources remaining in HDR safe, in the patient, or along transfer tubes);
- 1600 Treatments given to wrong patients;
- 1601 Treatments given to wrong cavities or orifices;
- Incorrectly prescribed or delivered doses, or repeated treatments to the same patient;
- Sources placed outside the transport safe and not secured;
- Damage in transit with failure to survey shipping packages;
- 1605 Inadequate shielding of brachytherapy procedure rooms;
- 1606 Source exchange accidents for HDR machines;
- 1607 Mechanical events associated with cables, kinks in applicators, stuck sources;
- 1608 Dislodged applicators;
- Treatment planning software errors;
- 1610 Failure of a retraction system; and
- Failure to adequately calibrate or recalibrate brachytherapy systems or sources.

(226) A collaborating team of specifically trained personnel following quality assurance
procedures is necessary to prevent accidents (See Section 5.7). Maintenance is an indispensable
component of QAP. External audits of procedures reinforce good and safe practice, and identify
potential causes of accidents. QAP should include peer review of cases. Accidents and incidents
should be reported, and the lessons learned should be shared with other users to prevent similar
mistakes (ICRP, 2000c, 2005a).

(227) *Publication 97* has addressed such exposures, events, and accidents for HDR
brachytherapy in some detail and should be consulted for the identification of prevention
methodologies (ICRP, 2005a).

1621 6.2. Emergency Procedures During and After Treatments

(228) Emergency procedures need to be developed for each brachytherapy procedure type
 (IAEA, 1998, 2001). Written procedures must be available on site and important information
 should be displayed prominently in the treatment room and control room, as needed. These
 procedures should be practised periodically to ensure emergency preparedness of the staff
 members. It is essential that the items required to perform emergency procedures are available



and remain in the brachytherapy suite, procedure room, or operating room prior to and duringall cases.

(229) The dose potentially received by both the patient and the staff may be very high in 1629 case of accidents if emergency procedures are not adapted or worse do not exist. Often, 1630 'immediate' (and not just 'quick') detection, presence of the responsible radiation oncologist, 1631 medical physicist, and therapist, is required, especially in HDR or PDR brachytherapy, where 1632 high doses can be delivered to patients or staff in seconds. For both patient and staff safety, 1633 there may be only a few minutes to recognise and event, react and resolve issues (Kaulich et 1634 al., 1999), and a very high standard of QA is mandatory. It is estimated that in such a case, the 1635 staff must react to correct the problem within 1-2 min. This minimal opportunity for mitigation, 1636 1637 by necessity, requires specific organisation and emergency response training (Kaulich et al., 1999). The swiftest possible rescue of a patient in an emergency and minimisation of staff 1638 exposures demands an unequivocal definition of responsibilities. It is advised that (as the 1639 organisational structure of the clinic allows), the emergency-responding physician should 1640 1641 preferably be the physician who placed the applicator. Clearly, a well-practiced emergency 1642 management can be of life-saving importance for the patient and can serve to minimise and 1643 mitigate potential exposures to staff.

(230) One of the most significant accidents in HDR brachytherapy occurred in 1992 in the 1644 U.S. during treatment of an anorectal cancer case. The source (HDR ¹⁹²Ir) became detached 1645 from the drive mechanism at the moment of the planned retraction of the source (which 1646 therefore remained in the patient). Unfortunately, the physicians in charge had to deal with 1647 1648 conflicting signals as the area radiation monitor actually detected the radiation, but the equipment (irradiator) indicated that the source had been shielded. In addition, radiation 1649 1650 monitor malfunctions in the months leading up to the accident encouraged misinterpretation 1651 and induced the staff not to trust the indications. Consequently, the wrong indication ('source shielded') of the equipment was accepted, and the patient, clothes and room were not 1652 subsequently checked with another radiation monitor or survey instrument. The HDR source 1653 1654 remained within the patient for 4 days, delivering a total dose of about 16,000 Gy (of note, the prescription was only for 18 Gy). The patient died on day 4. The catheter with the source went 1655 unrecognised, although it was removed from the patient along with necrotic tissues. This 1656 material was subsequently disposed of in a waste container, without identification of the source 1657 at that time. The waste container was picked up by a commercial medical waste disposal 1658 company 5 days later. It was then taken to an incinerator where the radiation monitor detected 1659 1660 the source, and the facility tracked the source back to the clinic, and the medical physicist was contacted. During the days the source remained in the patient or in the waste container, it 1661 irradiated 94 staff persons to various external dose levels (usually in only a few minutes). 1662

1663 (231) External audits of procedures re-enforce good and safe practice, and identify potential1664 causes of errors.

6.3. Emergency Surgery or Death of a Radioactive, LDR Brachytherapy Implanted Patient

1667 (232) If surgery is being contemplated for a patient receiving an LDR brachytherapy 1668 treatment, the radiation oncologist, medical physicist and radiation safety officer should be 1669 immediately notified. Temporary brachytherapy implants should be removed prior to any 1670 surgery needed by a patient. The radiation oncology team should give guidance to the surgical 1671 team during operations on patients with permanent implants.



1672 (233) If the patient should die while the radioactive sources are in place, the radiation 1673 oncologist, medical physicist, and radiation safety officer should be notified. The body should 1674 not be moved until these individuals arrive. If an autopsy is to be performed, it should be carried 1675 out only after the radioactive sources have been removed.

1676 (234) *Publication 98* (ICRP, 2005b) lists additional considerations with regard to cremation 1677 of a body containing LDR permanent implant sources noting that cremation can be allowed if 1678 12 months have elapsed since the implantation (while some countries set this delay at 3 y). If 1679 cremation is to be considered before that time, specific measures must be undertaken.

1680 6.4. Preventing Emergencies and Accidents

(235) An emergency plan should be prepared and practised with commencement of any
 brachytherapy procedure or operations. A list of emergency procedures (both medical and
 radiation) should be displayed prominently within the brachytherapy suite. All necessary
 emergency equipment items should be present. Training for all personnel should be repeated
 regularly, especially when new personnel are introduced to the team.

1686 (236) The person responsible for performing an emergency procedure should remain in the 1687 brachytherapy suite during the entire treatment. In some countries, it is a requirement that both 1688 a clinician and a medical physicist remain.

(237) General recommendations on preventing emergencies and accidents that could result 1689 in patient effects, member of the public, or occupational staff overexposures include several 1690 1691 considerations, such as a written comprehensive QA programme (See Section 5.7) and compliance with QA procedures. While not necessarily required by regulation, a hospital 1692 radiation safety committee (and perhaps a QA committee) needs to exist and interact with 1693 1694 regulatory and health authorities. Maintenance of equipment is extremely important. External 1695 audits of procedures should be performed to re-enforce good and safe practice, and identify potential causes of errors. All significant steps from prescription to final delivery of treatment 1696 1697 should be checked and verified by a second competent person. The objective is to ensure that the correct patient receives the correct dose at the correct site. Peer review of each case 1698 1699 improves quality. Every incident or accident should be reported as required to the appropriate 1700 authority.

(238) For HDR units, if a source comes away from the drive cable and lodges in a catheter
in the patient, the catheter should not be removed with an open end passing through the patient
since the source could leave the catheter an end up in the patient's tissues. Approaches to such
events must be planned by the facility before interstitial patients are treated and emergency
steps practiced.

(239) Training at a centre with experience in specific brachytherapy modalities (e.g. LDR
or HDR) should commence prior to machine acquisition and should include the specific
techniques to be used.

(240) Training should be directed towards ensuring a team approach involving a radiation
oncologist, a medical physicist, a technician, and a nurse. Emergency plan should be exercised
frequently.

(241) Source transportation should adhere to all applicable regulations. On site, shipping
 containers should be inspected for damage. For HDR brachytherapy sources, removal of old
 sources, their transfer to the container, and installation of new sources into appropriate shielded
 safes should be performed with care and by factory-trained and certified operators.



1716 (242) So-called 'false alarms' and interlock 'failures' should be taken seriously and 1717 investigated thoroughly, and appropriate action should be taken. Failure to do so may 1718 encourage staff to ignore valid alarm signals.

(243) Survey of the patient by a portable radiation monitor is essential after each treatment.
(244) For HDR machines and sources, particular attention should be paid if the facility or
machine is decommissioned to prevent the source from ending up in a junk yard or included in
scrap metal.

(245) It is extremely important that there be immediate local reporting and analysis of all
accidents. This should be followed by the identification of causes, contributing factors, and
extent of conditions; all of which should result in corrective measures. Responses to such
situations should be followed by rapid and widespread circulation of the relevant information,
to avoid similar problems being reproduced in another centre.

1728 (246) All procedures should undergo risk analysis and assessment of the quality 1729 management procedures in place to prevent events (Huq et al., 2016).



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REFERENCES

- Adkison, J.B., Thomadsen, B.R., Howard, S.P., 2008. Systemic iodine-125 activity after GliaSite 1732 brachytherapy: safety considerations. Brachytherapy 7:43-46. 1733
- Ahmed, S., Zimmer, A., McDonald, N., et al., 2007. The effectiveness of lead aprons in reducing 1734 radiation exposures from specific radionuclides. J. Nucl. Med. Meeting Abstr.48, 470. 1735
- Alazzoni, A., Gordon, C.L., Syed, J., et al., 2015. Randomized controlled trial of radiation protection 1736 1737 with a patient lead shield and a novel, nonlead surgical cap for operators performing coronary angiography or intervention. Circ. Cardiovasc. Interv. Aug;8(8), e002384. 1738
- 1739 Alvarado, M., Gallant, E., Rice, J., et al., 2015. A registry of targeted intraoperative radiation therapy 1740 following breast-conserving surgery. J Clin Oncol 33.
- Andrews, C., Walker, S., Ackermann, R., et al., 1994. Hepatic Radioembolization with Yttrium-90 1741 Containing Glass Microspheres: Preliminary Results and Clinical Follow-Up. J. Nucl. Med. 35, 1742 1743 1637–1644.
- Aparici, C.M., Win, A.Z., 2014a. Use of positron emission tomography/CT to perform biopsy of a 1744 1745 mesenteric mass. J. Vasc. Interv. Radiol.25, 1609.
- Aparici, C., Aslam, R., Win A., 2014b. Initial experience of utilizing real-time intra-procedural PET/CT 1746 1747 Biopsy. J. Clin. Imaging. Sci. 4, 54.
- 1748 Arazi, L., Cooks, T., Schmidt, M., et al., 2007. Treatment of solid tumours by interstitial release of 1749 recoiling short-lived alpha emitters. Phys Med Biol. 52:5025-5042.
- Aronowitz, J.N., 2002. Buried emanation: the development of seeds for permanent 1750 1751 implantation.Brachytherapy. 2002;1:167-178.
- Aronowitz, J.N., 2012. Whitmore, Henschke, and Hilaris: the reorientation of prostate brachytherapy 1752 1753 (1970-1987). Brachytherapy. 11(2):157-162.
- 1754 Artschan, R.E.R., Brettle, D.S., Chase, K., et al., 2014. An investigation of the radiation doses to the 1755 lower legs and feet of staff undertaking interventional procedures. Br. J. Radiol. 87, 20130746.
- Aubert, B., Guilabert, N., Lamon, A., et al., 2003. Which protection against radiation for new protocols 1756 of internal radiotherapy by Yttrium-90? 6th European ALARA Network Workshop. Madrid, 2002; 1757 1758 ISBN: 84-7834-437-3. Proceedings edited by CIEMAT, Madrid 2003.
- Badal, A., Zafar, F., Dong, H., et al., 2013. A real-time radiation dose monitoring system for patients 1759 and staff during interventional fluoroscopy using a GPU-accelerated Monte Carlo simulator and an 1760 1761 automatic 3D localization system based on a depth camera. Published as SPIE proceedings 1762 Proceedings Vol. 8668: Medical Imaging 2013: Physics of Medical Imaging.
- Balter, S., 1999. Radiation safety in the cardiac catheterization laboratory: basic principles. Catheter. 1763 Cardiovasc. Interv.47, 229-236 55. 1764
- Balter, S., 2001. Interventional fluoroscopy: Physics, technology, safety. Wiley-Liss, New York. 1765
- 1766 Balter, S., Lamont, J., 2002. Radiation and the pregnant nurse. Cath Lab Digest 10.
- Balter, S., Oetgen, M., Hill, A., et al., 2000. Personnel exposure during gamma endovascular 1767 1768 brachytherapy. Health Phys. 79(2):136-146.
- 1769 Bartal, G., Vañó, E., Paulo, G., et al., 2013. Management of Patient and Staff Radiation Dose in 1770 Interventional Radiology: Current Concepts. Cardiovasc. Intervent. Radiol. DOI 10.1007/s00270-1771 013-0685-0.
- 1772 Behrens, R., Dietze, G., 2010. Monitoring the eye lens: which dose quantity is adequate? Phys. Med. 1773 Biol. 55, 4047–4062.
- 1774 Behrens, R., Dietze, G., 2011. Dose conversion coefficients for photon exposure of the human eye lens. 1775 Phys. Med. Biol. 56, 415–437.
- Behrens, R., 2012a. Air kerma to Hp(3) conversion coefficients for a new cyclindrical phantom for 1776 1777 photon reference radiation qualities. Radiat. Prot. Dosim. 151, 450-455.
- Behrens, R., 2012b. On the operational quantity Hp(3) for eye lens dosimetry. J. Radiol. Prot. 32, 455-1778 1779 464.
- Beijst, C., Elschot, M., Viergever, M.A., et al., 2016. Toward Simultaneous Real-Time Fluoroscopic 1780 1781 and Nuclear Imaging in the Intervention Room. Radiology 278, 232-238.



- Benatar, N.A., Cronin, B.F., O'Doherty, M.J., 2000. Radiation dose rates from patients undergoing
 PET: implications for technologists and waiting areas. Eur. J. Nucl. Med.27, 583–589.
- Berrington de González, A., Ntowe, E., Kitahara, CM., et al., 2016. Long-term Mortality in 43763 U.S.
 Radiologists Compared with 64990 U.S. Psychiatrists. Radiology. 281. 847-857.
- Best, P.J., Skelding, K.A., Mehran, R., et al., 2011. SCAI consensus document on occupational radiation
 exposure to the pregnant cardiologist and technical personnel. EuroIntervention. 6, 866–874.
- Bester, L., Meteling, B., Pocock, N., et al., 2012. Radioembolization versus standard care of hepatic
 metastases: comparative retrospective cohort study of survival outcomes and adverse events in
 salvage patients.J. Vasc. Interv. Radiol. 23, 96–105.
- Bhatnagar, A., 2013. Nonmelanoma skin cancer treated with electronic brachytherapy: results at 1 year.
 Brachytherapy 12:134-140.
- Bilski, P., Bordy J-M., Daures, J., et al., 2011. The new EYE-D dosemeter for measurements of Hp(3)
 for medical staff. Rad. Measurements. 46. 1239-1242.
- Blake, M.E., Oates, M.E., Applegate, K., et al., 2006. Proposed program guidelines for pregnant
 radiology residents: a project supported by the American Association of Women Radiologists and
 the Association of Program Directors in Radiology. Acad. Radiol. 13, 391–401.
- Bolch, W.E., Dietze, G., Petoussi-Henss, N., et al., 2015. Dosimetric models of the eye and lens of the
 eye and their use in assessing dose coefficients for ocular exposures. Ann ICRP. 44(1 Suppl):91111.
- Buls, N., Pagés, J., de Mey, J., et al., 2003. Evaluation of patient and staff doses during various CT
 fluoroscopy guided interventions. Health Phys. 85, 165–173.
- Buls, N., Covens, P., Nieboer, K., et al., 2009. Dealing with pregnancy in radiology: a thin line between
 science, social and regulatory aspects. JBR-BTR 92, 271–279.
- Butler, W.M., Huq, M.S., Li, Z., et al., 2006. Third party brachytherapy seed calibrations and physicist
 responsibilities. [Letter] Mel Phys 33, 247-248.
- Cantone, M.C., Ginjaume, M., Miljanic, S., et al., 2017. Report of IRPA task group on the impact of
 the eye lens dose limits. J. Radiol. Prot. 37, 527–550.
- 1809 Carlson, S.K., Felmlee, J.P., Bender, C.E., et al., 2005. CT fluoroscopy-guided biopsy of the lung or
 1810 upper abdomen with a breath-hold monitoring and feedback system: a prospective randomized
 1811 controlled clinical trial. Radiol. 237, 701–708.
- 1812 Camacho, J.C., Moncayo, V., Kokabi, N., et al., 2015. 90Y Radioembolization: Multimodality Imaging
 1813 Pattern Approach with Angiographic Correlation for Optimised Target Therapy Delivery.
 1814 RadioGraphics 35, 1602–1620.
- 1815 Carinou, E., Ferrari, P., Koukorava, C., et al., 2011. Monte Carlo calculations on extremity and eye lens
 1816 dosimetry for medical staff at interventional radiology procedures. Radiat. Prot. Dosim.144, 492–
 1817 496.
- 1818 Carinou, E., Ferrari, P, Bjelac, O.C., et al., 2015. Eye lens monitoring for interventional radiology
 1819 personnel: dosemeters, calibration and practical aspects of Hp(3) monitoring. A 2015 review. J.
 1820 Radiol. Prot. 35. R17–34.
- Chambers, C.E., Fetterly, K.A., Holzer, R., et al., 2011.Radiation safety program for the cardiac
 catheterization laboratory. Catheter. Cardiovasc. Interv. 77, 546–556.
- 1823 Chiesa, C., 1997. Radiation dose to technicians per nuclear medicine procedure: Comparison between
 1824 technetium-99m, gallium-67, and iodine-131 radiotracers and fluorine-18 fluorodeoxyglucose. Eur.
 1825 J. Nucl. Med. 24, 1380–1389.
- 1826 Chiriotti, S., Ginjaume, M., Vañó. E., et al., 2011. Performance of several active personal dosimeters
 1827 in interventional radiology and cardiology. Rad. Measurements 46, 1266e1270.
- 1828 Christodoulou, E.G., Goodsitt, M.M., Larson, S.C., et al., 2003. Evaluation of the transmitted exposure
 1829 through lead equivalent aprons used in a radiology department, including the contribution from
 1830 backscatter. Med. Phys. 30, 1033.
- 1831 Ciraj-Bjelac, O., Rehani, M.M., Sim, K.H., et al., 2010. Risk for radiation-induced cataract for staff in
 1832 interventional cardiology: is there reason for concern? Catheter. Cardiovasc. Interv. 76, 826–834.



- 1833 Ciraj-Bjelac, O., Rehani, M.M., Minamoto, A., et al., 2012. Radiation-induced eye lens changes and
 1834 risk for cataract in interventional cardiology. Cardiology.123, 168–71.
- Clairand, I., Bordy, J-M., Carinou, E., et al., 2011. Use of active personal dosimeters in interventional
 radiology and cardiology: Tests in laboratory conditions and recommendations ORAMED project.
 Radiat. Meas. 46, 1252–1257.
- 1838 Classic, K.L., Furutani, K.M., Stafford, S.L., et al., 2012. Radiation dose to the surgeon during plaque
 1839 brachytherapy. Retina. 32(9):1900-1905.
- 1840 Clements, J., Moirano, J., Sherry, C., et al., 2015. Best practices for evaluating and tracking protective
 1841 garments. J. Am. Coll. Radiol. 12, 531–532.
- 1842 Clerinx, P., Buls, N., Bosmans, H., et al., 2008. Double-dosimetry algorithm for workers in
 1843 interventional radiology. Rad. Prot. Dosim. 129, 321–327.
- 1844 CNSC, 2017. Radionuclide information booklet. Canadian Nuclear Safety Commission: Ottawa.
- 1845 Cohen, G.N., Munro, J.J., Kirov, A., et al., 2014. 32P brachytherapy conformal source model RIC-100
 1846 for high-dose-rate treatment of superficial disease: monte carclo calculations, diode measurements,
 1847 and clinical implementation. Int J Rad Onc Bio Phys. 88(3):746-752.
- 1848 Cooks, T., Tal, M., Raab, S., et al. 2012. Intratumoral 224Ra-loaded wires spread alpha-emitters inside
 1849 solid human tumours in athymic mice achieving tumor control. Anticancer Res 32:5315-5322.
- Cousin, A.J., Lawdahl, R.B., Chakraborty, D.P., et al., 1987. The case for radioprotective
 eyewear/facewear. Practical implications and suggestions. Invest. Radiol. 22, 688–692.
- 1852 CRCPD, 2001. Conference of Radiation Control Program Directors, Inc. in Cooperation with Center
 1853 for Devices and Radiological Health of the Food and Drug Administration, 2001. Quality control
 1854 recommendations for diagnostic radiography. Vol. 3 Radiographic or fluoroscopic machines.
 1855 CRCPD, Kentucky.
- 1856 Cruzate, J., Discacciatti, A., 2008. IRPA Refresher Course 18: Shielding of medical facilities. Shielding
 1857 design considerations for PET-CT facilities.
- 1858 Daly, B., Templeton, P.A., 1999. Real-time CT fluoroscopy: evolution of an interventional tool.
 1859 Radiology 211, 309–315.
- Dauer, L.T., Miller, D.L., Schueler, B., et al., 2015. Occupational radiation protection of pregnant or
 potentially pregnant workers in IR: a joint guideline of the Society of Interventional Radiology and
 the Cardiovascular and Interventional Radiological Society of Europe. J. Vasc. Interv.Radiol. 26,
 171–181.
- 1864 Daures, J., Gouriou, J., Bordy, J.M., 2009. Conversion coefficients from air Kerma to personal dose
 1865 equivalent Hp(3) for eye-lens dosimetry. CEA Report CEA-R-6235 Saclay CEA.
- 1866 Day, M.J., Forster, E., 1981. Protective effect of spectacles. Brit. J. Radiol. 54, 137–138.
- 1867 Demir, M., Demir, B., Sayman, H., et al., 2010. Radiation protection for accompanying person and
 radiation workers in PET/CT. Radiat. Prot. Dosim. 147, 528–532.
- 1869 Detorie, N., Mahesh, M., Schueler, B.A., 2007. Reducing occupational exposure from fluoroscopy. J.
 1870 Am. Coll. Radiol. 4, 335–337.
- 1871 Deufel, C.L., Courneyea, L.A., McLemore, L.B., et al., 2015. Experimental and theoretical dosimetry
 1872 of the RIC-100 phosphorus-32 brachytherapy source for implant geometries encountered in the
 1873 intraoperative setting. Brachytherapy. 14(5):734-750.
- 1874 Devlin, P.M., Gaspar, L.E., Buzurovi, I., et al., 2017. American College of Radiology American
 1875 Brachytherapy Society practice parameter for electronically generated low-energy radiation sources.
 1876 Brachytherapy 16:1083-1090.
- 1877 Dewitt, K.D., Hsu, I.C., Speight, J., et al., 2005. 3D inverse treatment planning for the tandem and ovoid
 1878 applicator in cervical cancer. Int J Radiation Oncol Biol Phys. 63(4):1270-4.
- 1879 Dromi, S., Wood, B.J., Oberoi, J., et al., 2006. Heavy metal pad shielding during fluoroscopic
 1880 interventions. J. Vasc. Interv. Radiol. 17, 1201–1206.
- 1881 Durán, A., Hian, S.K., Miller, D.L., et al., 2013. Recommendations for occupational radiation protection
 1882 in interventional cardiology. Catheter. Cardiov. Interv. 82, 29–42.
- 1883 Eaton, D.J., 2015. Electronic brachytherapy current status and future directions. Br J Radiol
 1884 88:20150002.



- 1885 EC, 2015. Medical Radiation Exposure of the European Population Radiation Protection. No. 180.
- Eder, H., Schlattl, H., Hoeschen, C., 2010. X-ray protective clothing: Does DIN 6857-1 allow an
 objective comparison between lead-free and lead-composite materials? Fortschr.Röntgenstr. 182,
 422–428.
- 1889 Efstathopoulos, E.P., Pantos, I., Andreou, M., et al., 2011. Occupational radiation doses to the 1890 extremities and the eys in interventional radiology and cardiology. Brit. J. Radiol. 84, 70–77.
- Elschot, M., De Wit, T., De Jong H., 2010. The influence of self absorption on PET and PET/CT
 shielding requirements. Med. Phys. 37, 2999–3007.
- Faulkner, K., Marshall, N.W., 1993. Personal monitoring of pregnant staff in diagnostic radiology. J.
 Radiol. Prot. 13, 259.
- Faulkner, K., Werduch, A., 2008. Analysis of the frequency of interventional cardiology in various
 European countries. Radiat. Prot. Dosim. 129, 74–76.
- Felmlee, J.P., McGough, P.F., Morin, R.L., et al., 1991. Hand dose measurements in interventional
 radiology. Health Phys. 60, 265–267.
- Fetterly, K., Schueler, B., Grams, M., et al., 2017. Head and Neck Radiation Dose and Radiation Safety
 for Interventional Physicians JACC Cardiovasc Interv. 2017 Mar 13;10(5):520-528.
- Fischman, A.M., Ward, T.J., Patel, R.S., et al., 2014. Prospective, randomized study of coil
 embolization versus Surefire infusion system during yttrium-90 radioembolization with resin
 microspheres. J. Vasc. Interv. Radiol.25, 1709–1716.
- Finnerty, M., Brennan, P.C., 2005. Protective aprons in imaging departments: manufacturer stated lead
 equivalence values require validation. Eur. Radiol. 15, 1477–1484.
- Franken, Y., 2002. Guidance on the use of protective lead aprons in medical radiology protection
 efficiency and correction factors for personal dosimetry. Proc. 6th European ALARA Network
 Workshop. Occupational exposure optimisation in the medical field and radiopharmaceutical
 industry. Madrid, 135–139.
- Galster, M., Guhl, C., Uder, M., et al., 2013. Exposition of the Operator's Eye Lens and Efficacy of
 Radiation Shielding in Fluoroscopically Guided Interventions. RoFo. 185, 474–481.
- Geber, T., Gunnarsson, M., Mattsson. S., 2012. Eye lens dosimetry for interventional procedures –
 Relation between the absorbed dose to the lens and dose at measurement positions. Radiation
 Measurements Volume 46, Issue 11, Pages 1248-1251.
- 1915 GEC ESTRO, 2018. The GEC ESTRO Handbook of Brachytherapy, 2nd Ed. Limbergen, E.V., Potter,
 1916 R., Hoskin, P., Baltas, D. Eds. European Society for Radiotherapy & Oncology.
 1917 https://www.estro.org/about/governance-organisation/committees-activities/gec-estro-handbook 1918 of-brachytherapy
- Gianfelice, D., Lepanto, L., Perreault, P., et al., 2000a. Effect of the learning process on procedure times
 and radiation exposure for CT fluoroscopy-guided percutaneous biopsy procedures. J. Vasc.
 Interv.Radiol. 11, 1217–1221.
- Gianfelice, D., Lepanto, L., Perreault, P., et al., 2000b. Value of CT fluoroscopy for percutaneous
 biopsy procedures. J. Vasc. Interv. Radiol. 11, 879–884.
- Goodney, P.P., Beck, A.W., Nagle, J., et al., 2009. National trends in lower extremity bypass surgery,
 endovascular interventions, and major amputations. Journal of vascular surgery: official publication,
 the Society for Vascular Surgery [and] International Society for Cardiovascular Surgery, North
 American Chapter 50, 54–60.
- Guersen, J., Cassagnes, L., Mechin, G., et al., 2013. Interventional radiologists: a necessary evolution
 of leaded protective aprons design. Journal of vascular and interventional radiology: JVIR 24, 443.
- Hagspiel, K.D., Nambiar, A., Hagspiel, L.M., et al., 2013. Temporary arterial balloon occlusion as an
 adjunct to yttrium-90 radioembolization. Cardiovasc. Intervent. Radiol. 36, 809–813.
- Harris, T.J., Zafar, A.M., Murphy, T.P., 2011. Utilization of lower extremity arterial disease diagnostic
 and revascularization procedures in Medicare beneficiaries 2000-2007.AJR. Am. J. Roentgenol. 197,
 W314-317.
- 1935 Haskal, Z.J., 2004. Interventional radiology carries occupational risk for cataracts. RSNA News, June
- 1936 2004. http://www.barrieronline.com/info/RSNAreprint.pdf.



- Häusler, U., Czarwinski, R., Brix, G., 2009. Radiation exposure of medical staff from interventional xray procedures: a multicentre study. Eur. Radiol. 19, 2000-2008.
- Heckathorne, E., Dahlbom M., 2008. Radiation dose to surgical staff from positron-emitter-based
 localization and radiosurgery of tumours. Health Phys. 95, 220–226.
- Hilaris, B.S., Batata, M.E., Anderson, L.L., 1987. Chapter 26. In: Pierquin, B., Wilson, J.F., Chassagne,
 D.(Eds.), Prostate in Modern Brachytherapy. Masson, New York, pp. 234–247.
- Hiles, P.A., Hughes, H., Arthur, D., et al., 2016. Personal protective equipment. British Institute ofRadiology, London.
- Hill, K.D., Frush, D.P., Han, B.K., et al., 2017. Radiation safety in children with congenital and acquired
 heart disease: a scientific position statement on multimodality dose optimization from the image
 gently alliance. JACC Cardiovasc. Imaging. 10. 797-818.
- Hippelainen, E., Nikkinen, P., Ihalainen, T., et al., 2008. Personal radiation doses in PET/CT facility:
 measurements vs. calculations. Radiat. Prot. Dosim. 132, 57–63.
- Hoang, J.K., Yoshizumi, T.T., Toncheva, G., et al., 2011. Radiation dose exposure for lumbar spine
 epidural steroid injections: a comparison of conventional fluoroscopy data and CT fluoroscopy
 techniques. AJR. Am. J. Roentgenol. 197, 778–782.
- Holland, J., Williamson, M., Lewis, J., 2010. Unconventional nuclides for radiopharmaceuticals. Mol.
 Imaging. 9, 1–20.
- Hu, P., Kong, Y., Chen, B., et al., 2017. Shielding effect of lead glasses on radiologists' eye lens
 exposure in interventional procedures. Rad. Prot. Dosim. 174. 136-140.
- Huq, M. S., Fraass, B. A., Dunscombe, B. A., et al., 2016. The report of Task Group 100 of the AAPM:
 Application of risk analysis methods to radiation therapy quality management. Med. Phys. 43, 42094262. doi: 10.1118/1.4947547.
- IAEA, 2001. Implementation of microsource high dose rate (mHDR) brachytherapy in developing
 countries. IAEA-TECDOC-1257. International Atomic Energy Agency: Vienna.
- IAEA, 2002. Calibration of photon and beta ray sources used in brachytherapy. IAEA-TECDOC-1274.
 Vienna: International Atomic Energy Agency.
- IAEA, 2005. Radiation oncology physics: a handbook for teachers and students. Podgorsak, E.B.,
 technical ed. Vienna: International Atomic Energy Agency.
- IAEA, 2006. Design of radiotherapy facilities. IAEA Safety Series No. 47. International Atomic Energy
 Agency: Vienna.
- IAEA, 2008. Setting up a radiotherapy programme: clinical, medical physics, radiation protection and
 safety aspects. STI/PUB/1296. International Atomic Energy Agency, Vienna.
- IAEA, 2013. International Atomic Energy Agency. Implications for occupational radiation protection
 of the new dose limit for the lens of the eye. IAEA-TECDOC-1731. IAEA, Vienna.
- IAEA, 2014a. European Commission, Food and Agriculture Organization of the United Nations,
 International Atomic Energy Agency, International Labour Organization, Oecd Nuclear Energy
 Agency, Pan American Health Organization, United Nations Environment Programme, World
 Health Organization, Radiation Protection and Safety of Radiation Sources: International Basic
- 1976 Safety Standards, IAEA Safety Series No. GSR Part 3, IAEA, Vienna.
- IAEA, 2014b. Recommendations of the Working Group on Interventional Cardiology on occupational
 doses to the lens of the eye in Interventional Cardiology, The Information System on Occupational
 Exposure in Medicine, Industry and Research (ISEMIR): IAEA -TECDOC-1735. IAEA, Vienna.
- IAEA, 2016. Web site on Radiation protection of patients. Last entry September 2016.
 https://rpop.iaea.org/RPOP/RPoP/Content/News/relid-activities.htm.
- ICRP, 1990. Rradiological protection of the worker in medicine and dentistry. ICRP Publication 57,
 Ann. ICRP 20(3).
- ICRP, 1991. 1990 Recommendations of the International Commission on Radiological Protection.
 ICRP Publication 60. Ann. ICRP 21(1-3).
- ICRP, 1996. Conversion coefficients for use in radiological protection against external radiation. ICRP
 Publication 74. Ann. ICRP 26(3/4).
- 1988 ICRP, 2000a. Pregnancy and medical radiation. ICRP Publication 84. Ann. ICRP 30(1).



- ICRP, 2000b. Avoidance of radiation injuries from medical interventional procedures. ICRP
 Publication 85. Ann. ICRP 30(2).
- 1991 ICRP, 2000c. Prevention of accidents to patients undergoing radiation therapy. ICRP Publication 86.1992 Ann. ICRP 30(3).
- ICRP, 2005a. Prevention of high-dose rate brachytherapy accidents. ICRP Publication 97. Ann. ICRP
 35(2).
- ICRP, 2005b. Radiation safety aspects of brachytherapy for prostate cancer using permanently
 implanted sources. ICRP Publication 98. Ann. ICRP 35(3).
- ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection.
 ICRP Publication 103. Ann. ICRP 37(2-4).
- 1999 ICRP, 2008. Radiological protection in medicine. ICRP Publication 105. Ann. ICRP 37(6).
- ICRP, 2009. Education and training in radiological protection for diagnostic and interventional
 procedures. ICRP Publication 113, Ann. ICRP 39(5).
- ICRP, 2010a. Radiological protection in fluoroscopically guided procedures performed outside the
 imaging department. ICRP Publication 117, Ann. ICRP 40 (6).
- ICRP, 2010b. Conversion Coefficients for Radiological Protection Quantities for External Radiation
 Exposures. ICRP Publication 116, Ann. ICRP 40(2–5).
- ICRP, 2010c. Preventing accidental exposures from new external beam radiation therapy technolgoies.
 ICRP Publication 112. Ann. ICRP 39(4).
- 2008 ICRP, 2011. Statement on tissue reactions. ICRP ref. 4825-3093-1464, April 21, 2011.
- ICRP, 2012. ICRP statement on tissue reactions and early and late effects of radiation in normal tissues
 and organs threshold doses for tissue reactions in a radiation protection context. ICRP Publication
 118, Ann. ICRP 41(1/2).
- 2012 ICRP, 2013a. Radiological protection in cardiology. ICRP Publication 120.Ann. ICRP 42 (1).
- ICRP, 2013b. Radiological Protection in Paediatric Diagnostic and Interventional Radiology. ICRP
 Publication 121, Ann ICRP 42(2).
- ICRP, 2018. Occupational radiological protection in interventional procedures. ICRP Publication 139,
 Ann ICRP 47(2).
- ICRP, 2019. Radiological protection in therapy with radiopharmaceuticals. ICRP Publication 140. Ann
 ICRP 48(1).
- ICRU, 1997. Dose and Volume Specification for Reporting Interstitial Therapy. ICRU Report 58.
 International Commission on Radiation Units and Measurements, Bethesda, MD.
- ICRU, 2013. Prescribing, Recording, and Reporting Brachytherapy for Cancer of the Cervix: Report
 89. International Commission on Radiation Units and Measurements, Bethesda, MD.
- IEC, 2005. International Electrotechnical Commission. Medical diagnostic x-ray equipment-radiation
 conditions for use in the determination of characteristics IEC 61267, Geneva-IEC.
- IEC, 2012. Radiation protection instrumentation Passive integrating dosimetry systems for personal
 and environmental monitoring of photon and beta radiation. International Electrotechnical
 Commission. IEC- 62387. ed1.0.
- IEC, 2014. Protective devices against diagnostic medical X-radiation Part 1: Determination of attenuation properties of materials. IEC 61331-1, ed 2.
- IRPA, 2017. IRPA guideline protocol for eye dose monitoring and eye protection of
 workers.http://www.sppcr.pt/site/assets/files/1068/irpa_guidance_on_implementation_of_eye_dos
 e monitoring 2017.pdf
- IRSN, Institut de Radioprotection et Sureté Nucleaire. http://dosimetre.irsn.fr/fr fr/Documents/Fiches%20produits/IRSN_Fiche_dosimetre_Cristallin.pdf. Le dosimètre cristallin
 DOSIRIS. Last visited 15-07-2017.
- ISO, 1996. International Organization for Standardization. X-ray and gamma reference radiation for
 calibrating dosimeters and dose rate meters and for determining their response as a function of
 photon energy: part 1. Radiation characteristics and production methods ISO 4037-1, Geneva-IEC.
- ISO, 2015. International Organization for Standardization. Radiological protection: procedures for monitoring the dose to the lens of the eye, the skin and the extremities. ISO 15382 (2nd ed.).



- Jacob, S., Boveda, S., Bar, O., et al., 2012. Interventional cardiologists and risk of radiation-induced
 cataract: Results of a French multicenter observational study. Int. J. Cardiol. 167, 1843–1847.
- Jacob, S., Donadille, L., Maccia, C., et al., 2013. Eye lens radiation exposure to interventional cardiologists: a retrospective assessment of cumulative doses. Rad. Prot. Dosim. 153, 282–293.
- Jakobs, T.F., Hoffmann, R.T., Poepperl, G., et al. 2007. Mid-term results in otherwise treatment
 refractory primary or secondary liver confined tumours treated with selective internal radiation
 therapy (SIRT) using 90Yttrium resin-microspheres. Eur. Radiol. 17, 1320–1330.
- Järvinen, H., Buls, N., Clerinx, P., et al., 2008. Overview of double dosimetry procedures for the determination of the effective dose to the interventional radiology staff. Rad. Prot. Dosim. 129, 333–339.
- Joemai, R.M., Zweers, D., Obermann, W.R., et al., 2009. Assessment of patient and occupational dose
 in established and new applications of MDCT fluoroscopy. Am. J. Roentgenol. 192, 881–886.
- Junk, A.K., Haskal, Z., Worgul, B.V., 2004. Cataract in interventional radiology an occupational
 hazard? Invest. Ophthalmol. Vis. Sci. 45(Suppl. 1):U178.
- Kaulich, T.W., Becker, G., Lamprecht, U., et al., 1999. Emergency rescue in accidents with HDR
 afterloading units. Strahlenther Onkol. 175(10):524-9.
- Kemerink, G.J, Vanhavere, F., Barth, I., et al., 2012. Extremity doses of nuclear medicine personnel: a
 concern. Eur. J. Nucl. Med. Mol. Imaging. 39, 529–532.
- Kicken, P.J.H., Kemerink, G.J., van Engelshoven, J.M.A., 1999a. Dosimetry of occupationally exposed
 persons in diagnostic and interventional arteriography. Part I: Assessment of entrance doses. Rad.
 Prot. Dosim. 82, 93–103.
- Kicken, P.J.H., Kemerink, G.J., Schultz, F.W., et al., 1999b. Dosimetry of occupationally exposed
 persons in diagnostic and interventional arteriography. Part II: Assessment of effective dose. Rad.
 Prot. Dosim. 82, 105–114.
- Kim, K.P., Miller, D.L., Balter, S., et al., 2008. Occupational radiation doses to operators performing
 cardiac catheterization procedures. Health Phys. 94, 211–227.
- Kim, K.P., Miller, D.L., 2009. Minimising radiation exposure to physicians performing
 fluoroscopically guided cardiac catheterisation procedures: a review. Radiat. Prot. Dosim. 133, 227–
 2069 233.
- Kim, G.R., Hur, J., Lee, S.M., et al., 2011. CT fluoroscopy-guided lung biopsy versus conventional CT guided lung biopsy: a prospective controlled study to assess radiation doses and diagnostic
 performance. Eur. Radiol. 21, 232–239.
- Kim, K.P., Miller, D.L., Berrington de Gonzalez, A., et al., 2012. Occupational radiation doses to
 operators performing fluoroscopically-guided procedures. Health Phys. 103, 80–99.
- Kitahara1, C.M., Linet, M.S., Balter, S., et al., 2017. Occupational Radiation Exposure and Deaths
 From Malignant Intracranial Neoplasms of the Brain and CNS in U.S. Radiologic Technologists,
 1983–2012. AJR 2017; 208. 1278–1284.
- King, J.N., Champlin, A.M., Kelsey, C.A., et al., 2002. Using a sterile disposable protective surgical
 drape for reduction of radiation exposure to interventionalists. Am. J. Roentgenol. 178, 153–157.
- Klein, L.W., Miller, D.L., Balter, S., et al., 2009. Occupational health hazards in the interventional laboratory: time for a safer environment. J. Vasc. Interv. Radiol. 20, 147–152 quiz 153.
- Klein, L.W., Tra, Y., Garratt, K.N., et al., 2015. Occupational health hazards of interventional
 cardiologists in the current decade: Results of the 2014 SCAI membership survey. Catheter.
 Cardiovasc. Interv. 86, 913–924.
- Kollmeier, M.A., Stock, R.G., Stone, N., 2003. Biochemical outcomes after prostate brachytherapy with
 5-year minimal follow-up: importance of patient selection and implant quality. Int. J. Radiat. Oncol.
 Biol. Phys. 57, 645–653.
- Kong, Y., Struelen, L, Vanhavere, F., et al., 2015. Influence of standing positions and beam projections
 on effective dose and eye lens dose of anaesthetists in interventional procedures. Rad. Prot. Dosim.
 163, 181–187.
- Korir, G.K., Ochieng, B.O., Wambani, J.S., et al., 2012. Radiation exposure in interventional
 procedures. Radiat. Prot. Dosim. 152. 339–344.



- Koukorava, C., Carinou, E., Simantirakis, G., et al., 2011. Doses to operators during interventional radiology procedures: focus on eye lens and extremity dosimeters. Rad. Prot. Dosim. 144, 482–486.
- Koukorava, C., Farah, J., Struelens, L., et al., 2014. Efficiency of radiation protection equipment in
 interventional radiology: a systematic Monte Carlo study of eye lens and whole body doses. J. Radiol.
 Prot. 34, 509–528.
- Kramer, R., Zankl, M., Williams, G., et al., 1982. The male (ADAM) and female (EVA) adult
 mathematical phantoms. Neuherberg, Germany: Institut fuer Strahlenschutz, GSFForschungszentrum fuer Umwelt und Gesundheit. The calculation of dose from external photon
 exposures using reference human phantoms and Monte Carlo methods: Part I. GSF-Report S-885.
- Kubo, H.D., Glasgow, G.P., Pethel, T.D., et al., 1998. High dose-rate brachytherapy treatment delivery:
 report of the AAPM Radiation Therapy Committee Task Group No. 59. Medical Physic. 25:375-403
 (1998).
- Kuipers, G., Velders, X.L., De Winter, R.J., et al., 2008. Evaluation of occupational doses of
 interventional radiologists. Cardiovasc. Intervent. Radiol. 31, 483–489.
- Kuipers, G., Velders, X.L., 2009. Effective doses to staff from interventional procedures: estimations
 from single and double dosimetry. Radiat. Prot. Dosim. 136, 95–100.
- Jones, A.K., Wagner, L.K., 2013. On the (f)utility of measuring the lead equivalence of protective
 garments. Med. Phys. 40(6):063902.
- Laube, T., Fluhs, D., Kessler, C., et al., 2000. Determination of surgeon's absorbed dose in iodine 125
 and ruthenium 106 ophthalmic plaque surgery. Ophthalmology. 107(2):366-368.
- Leng, S., Christner, J.A., Carlson, S.K., et al., 2011. Radiation dose levels for interventional CT
 procedures. AJR. Am. J. Roentgenol. 197, W97-103.
- Lessard, E., Pouliot, J., 2001. Inverse planning anatomy-based dose optimization for HDRbrachytherapy of the prostate using fast simulated annealing algorithm an dedicated objective
 function. Med. Phys. 28(5):773-779.
- Lichliter, A., Weir, V., Heithaus, R.E., et al., 2017. Clinical evaluation of protective garments with
 respect to garment characteristics and manufacturer label information. J. Vasc. Interv. Radiol. 28,
 148–155.
- Lie, Ø.Ø., Paulsen, G.U., Wøhni, T., 2008. Assessment of effective dose and dose to the lens of the eye
 for the interventional cardiologist. Radiat. Prot. Dosim. 132. 313–318.
- Linet, M.S., Kitahara, C.S., Ntowe, E., et al., 2017. Mortality in U.S. Physicians Likely to Perform
 Fluoroscopy guided Interventional Procedures Compared with Psychiatrists, 1979 to 2008.
 Radiology. 284. 482-494.
- Loose, R., 2003, Occupational Overexposures in Medical Field in European Commission, RP 149,
 Proceedings of the EU Scientific Seminar 2003 "Medical Overexposures".
- Madsen, M.T., Anderson, J.A., Halama, J.R., et al., 2006. AAPM Task Group 108: PET and PET/CT
 shielding requirements. Med. Phys. 33, 4–15.
- McCann, J.W., Larkin, A.M., Martino, L.J., et al., 2012. Radiation emission from patients treated with
 selective hepatic radioembolization using Yttrium-90 microspheres: are contact restrictions
 necessary? J. Vasc. Interv. Radiol. 23, 661–667.
- Maeder, M., Brunner-La Rocca, H.P., Wolber, T., et al., 2006. Impact of a lead glass shieldshield on
 scatter radiation to eyes and hands in interventional cardiologists, Catheter. Cardiovasc. Interv. 67,
 18–23.
- Magee, J.S., Martin, C.J., Sandblom, V., et al., 2014. Derivation and application of dose reduction
 factors for protective eyewear worn in interventional radiology and cardiology. J. Radiol. Prot. 34,
 811–823.
- Mann, J.T. 3rd., Cubeddu, G., Arrowood, M., 1996. Operator Radiation Exposure in PTCA:
 Comparison of Radial and Femoral Approaches. J. Invasive Cardiol. 8 (Suppl D):22D-25D.
- Marchese, M.J., Nori, D., Anderson, L.L., et al., 1984. A versatile permanent planar implant technique
 utilizing iodine-125 seeds imbedded in gelfoam. Int. J. Radiat. Oncol. Biol. Phys. 10, 747–751.
- Marshall, N.W., Faulkner, K., Clarke P., 1992. An investigation into the effect of protective devices on
- 2144 the dose to radiosensitive organs in the head and neck. Br. J. Radiol. 65. 799-802.



- Martin, C.J., 2009. A review of radiology staff doses and dose monitoring requirements. Radiat. Prot.
 Dosim. 136, 140–157.
- Martin, C.J., 2012. Personnel dosimetry in UK radiology: is it time for a change? J. Radiol. Prot. 32,
 E3–E6.
- Martin, C.J., Magee, J.S., 2013. Assessment of eye and body dose for interventional radiologists, cardiologists, and other interventional staff. J. Radiol.Prot. 33, 445–460.
- Martin, C.J., 2016. Eye lens dosimetry for fluoroscopically guided clinical procedures: practical
 approaches to protection and dose monitoring. Rad. Prot. Dosim. 169, 286–291.
- Marx, M.V., Niklason, L., Mauger, E.A., 1992. Occupational radiation exposure to interventional
 radiologists: a prospective study. J. Vasc. Interv. Radiol. 3, 597–606.
- Mateya, C. F., Claycamp, H. G., 1997. Phantom-derived estimation of effective dose equivalent from
 X-rays with and without a lead apron. Health Phys. 72, 842–847.
- McCaffrey, J.P., Tessier, F., Shen, H., 2012. Radiation shielding materials and radiation scatter effects
 for interventional radiology (IR) physicians. Med. Phys. 39, 4537–4546.
- McEwan, A.C., 2000. Assessment of occupational exposure in New Zealand from personal monitoring
 records. Rad. Prot. (Australasia) 17, 60–66.
- McVey, S., Sandison, A., Sutton, D.G., 2013. An assessment of lead eyewear in interventional
 radiology. J. Radiol. Prot. 33, 647–659.
- McLoney, E., Isaacson, A., Keeting P., 2014. The role of PET imaging before, during, and after
 percutaneous hepatic and pulmonary tumor ablation. Semin. Intervent.Radiol. 31, 187–192.
- Michalski, J., Mutic, S., Eichling, J., et al., 2003. Radiation exposure to family and household members
 after prostate brachytherapy. Int. J. Radiat. Oncol. Biol. Phys. 56, 764–768.
- Miller, D.L., Vucich, J.J., Cope, C., 1985. A flexible shield to protect personnel during interventional
 procedures. Radiology 155, 825.
- Miller, D.L., Vañó, E., Bartal, G., et al., 2010. Occupational radiation protection in interventional radiology: a joint guideline of the Cardiovascular and Interventional Radiology Society of Europe and the Society of Interventional adiology. Cardiovasc. Intervent. Radiol. 33, 230–239.
- Minot, D.M., Jaben, E., Aubry, M.C., et al., 2012. Evolution of transthoracic fine needle aspiration and
 core needle biopsy practice: A comparison of two time periods, 1996-1998 and 2003-2005.
 Diagn.Cytopathol. 40, 876–881.
- Mobit, P.N., Rajaguru, P., Brewer, M., et al., 2015. Radiation safety consideration during intraoperative
 radiation therapy. Radiat Prot Dosim 164:376-382.
- Moore, W.E., Ferguson, G., Rohrmann, C., 1980. Physical factors determining the utility of radiation
 safety glasses. Med. Phys.7, 8–12.
- Morrish, O.W.E., Goldstone, K.E., 2008. An investigation into patient and staff doses from X-ray
 angiography during coronary interventional procedures. Brit. J. Radiol. 81, 35–45.
- Nath, R., Amols, H., Coffey, C., et al., 1999. Intravascular brachytherapy physics: Report of the AAPM
 Radiation Therapy Committee Task Group No. 60. Med. Phys. 26, 119-152.
- NA/NRC, 2006. National Academies/National Research Council. Health Risks from Exposure to Low
 Levels of Ionizing Radiation, BEIR VII, Phase 2 (National Academies Press, Washington).
- NCRP, 1993. Limitation of Exposure to Ionizing Radiation. NCRP Report No. 116. National Council
 on Radiation Protection and Measurements, Bethesda, MD.
- NCRP, 2005. Structural shielding design and evaluation for megavoltage x- and gamma-ray
 radiotherapy facilities. NCRP Report No. 151. National Council on Radiation Protection and
 Measurements, Bethesda, MD.
- NCRP, 2006. Management of radionuclide therapy patients. NCRP Report No. 155. National Council
 on Radiation Protection and Measurements, Bethesda, MD.
- NCRP, 2009. Ionizing radiation exposure of the population of the United States.NCRP Report No. 160.
 National Council on Radiation Protection and Measurements, Bethesda, MD.
- 2194 NCRP, 2010. Radiation dose management for fluoroscopically guided interventional medical
- 2195 procedures. NCRP Report No. 168. National Council on Radiation Protection and Measurements,2196 Bethesda, MD.



- NCRP, 2016. Guidance on radiation dose limits for the lens of the eye. Commentary No. 26. National
 Council on Radiation Protection and Measurements, Bethesda, Maryland.
- Niklason, L.T., Marx, M.V., Chan, H.P., 1993. Interventional radiologists: occupational radiation doses
 and risks. Radiology 187, 729–733.
- Nordion Inc., TheraSphere (yttrium-90 glass microspheres) [package insert]. Available at: https://www.btg-im.com/Therasphere/RoW, Accessed 3rd September, 2016.
- Nye, A., Dubose, M., Votaw, J., 2009. A comparison of AAPM TG-108 PET/CT shielding
 recommendations and measurements in an oncology center. Med. Phys. 36, 5017–5021.
- Ordiales, J.M., Nogales, J.M., Sánchez-Casanueva, R., et al., 2015. Reduction of occupational radiation
 dose in staff at the cardiac catheterisation laboratory by protective material placed on the patient.
 Radiat. Prot. Dosim. 165, 272–275.
- Osei, E.K., Kotre, C.J., 2001. Equivalent dose to the foetus from occupational exposure of pregnant
 staff in diagnostic radiology. Br. J. Radiol. 74, 629–637.
- Ouhib, Z., Kasper, M., Perez Calatayud, J., et al., 2015. Aspects of dosimetry and clinical practice of
 skin brachytherapy: the American Brachytherapy Society working group report. Brachytherapy
 14:840-858.
- Padovani, R., Le Heron, J., Cruz-Suarez, R., et al., 2011. International project on individual monitoring
 and radiation exposure levels in interventional cardiology. Radiat. Prot. Dosim. 144, 437–441.
- Papadopoulos, N., Papaefstathiou, C., Kaplanis, P.A., et al., 2009. Comparison of Lead-free and
 Confencional X-ray aprons for Diagnostic Radiology.International Federation of Medical and
 Biological Engineering (IFMBE) proceedings 25/III, 544–546.
- Papagioannis, P., Venselaar, J., 2014. Radiation Protection in Brachytherapy. In Part 1: The Basics of
 Brachytherapy in The GEC ESTRO Handbook of Brachytherapy, 2nd Ed. Limbergen, E.V., Potter,
 R., Hoskin, P., Baltas, D. Eds. European Society for Radiotherapy & Oncology.
- Pasciak, A.S., Kyle, J.A., Wagner, L.K., 2015. Application of the diagnostic radiological index of
 protection to protective garments. Med. Phys. 42, 653–662.
- Paulson, E.K., Sheafor, D.H., Enterline, D.S., et al., 2001. CT fluoroscopy-guided interventional
 procedures: techniques and radiation dose to radiologists. Radiol. 220, 161–167.
- 2225 Pelz, D.M., 2000. Low back pain, lead aprons, and the angiographer. Am. J. Neuroradiol.21, 1364.
- Politi, L., Biondi-Zoccai, G., Nocetti, L., et al., 2012. Reduction of scatter radiation during transradial
 percutaneous coronary angiography: A randomized trial using a lead-free radiation shield. Cath.
 Cardiovasc. Interv. 79, 97–102.
- Principi, S., Ginjaume, M., Duch, M.A., et al., 2014. Influence of dosimeter position for the assessment
 of eye lens dose during interventional cardiology. Radiat. Prot. Dosim. 164, 79–83.
- Principi, S., Soler, C.D., Ginjaume, M., et al., 2015. Eye lens dose in interventional cardiology. Rad.
 Prot. Dosim. 165, 289–293.
- Purandare, N., Rangarajan, V., Shah, S.A., et al., 2011. Therapeutic response to radiofrequency ablation
 of neoplastic lesions: FDG PET/CT findings. Radiographics 31, 201–213.
- Quinn, B., Dauer, Z., Pandit-Taskar, N., et al., 2016. Radiation dosimetry of 18F-FDG PET/CT:
 incorporating exam-specific parameters in dose estimates. BMC Med Imaging. 16:41.
- Rehani, M.M., Vañó, E., Ciraj-Bjelac, O., et al., 2011. Radiation and cataract. Radiat. Prot. Dosim. 147,
 300–304.
- Reeves, R.R., Ang, L., Bahadorani, J., et al., 2015. Invasive Cardiologists Are Exposed to Greater Left
 Sided Cranial Radiation. The BRAIN Study (Brain Radiation Exposure and Attenuation During
 Invasive Cardiology Procedures). J. Am. Coll. Cardiol. Intv. 8. 1197–206.
- Rimpler, A., Barth, I., 2007. Beta radiation exposure of medical staff and implications for extremity
 dose monitoring. Radiat. Prot. Dosim. 125, 335–339.
- Roguin, A., Goldstein, J., Bar, O., et al., 2013. Brain and neck tumours among physicians performing
 interventional procedures. Am. J. Cardiol. 111. 1368–1372.
- Ryan, E.R., Sofocleous, C.T., Schoder, H., et al., 2013a. Split-dose technique for FDG PET/CT-guided percutaneous ablation: a method to facilitate lesion targeting and to provide immediate assessment
- of treatment effectiveness. Radiology 268, 288–295.



- Ryan, E.R., Thornton, R., Sofocleous, C.T., et al., 2013b. PET/CT-guided interventions: personnel
 radiation dose. Cardiovasc. Instevent. Radiol. 36, 1063–1067.
- Safigholi, H., Song, W.Y., Meigooni, A.S., 2015. Optimum radiation source for radiation therapy of
 skin cancer. J Appl Clin Med Phys 16:5407.
- Saidatul, A., Azlan, C., Megat, A.M., et al., 2010. A survey of radiation dose to patients and operators
 during radiofrequency ablation using computed tomography. Biomedical imaging and intervention
 journal 6, e1. doi:10.2349/biij.6.1.e2.
- Sánchez, R.M., Vañó, E., Fernández, J.M., et al., 2012. Staff doses in interventional radiology: a national survey. J. Vasc. Interv.Radiol. 23, 1496–1501.
- Sánchez, R.M., Vañó, E., Fernandez, J.M., et al., 2014. Measurements of eye lens doses in interventional cardiology using OSL and electronic dosimeters. Radiat. Prot. Dosim. 162, 569–576.
- Sánchez, R.M., Vañó, E., Fernández, J.M., et al., 2015. Evaluation of an automated FDG dose infuser
 to PET-CT patients. Radiat. Prot. Dosim. 165, 457–460.
- Sandblom, V., 2012. Evaluation of Eye Lens Doses Received by Medical Staff Working in
 Interventional Radiology at Sahlgrenska University Hospital. MSc. Thesis. Department of Radiation
 Physics University of Gothenburg Gothenburg, Sweden.
- Sauren, L.D., Van Garsse, L., Van Ommen, V., et al., 2011. Occupational radiation dose during
 transcatheter aortic valve implantation. Cathet. Cardiov Interv. 78, 770–776.
- Savage, C., Carlson, L., Clements, J., et al., 2009. Comparison of the zero gravity system to
 conventional lead apron for radiation protection of the interventionalist. J. Vasc. Interv. Radiol.20,
 S53.
- Schiefer, H., von Toggenburg, F., Seelentag, W., et al., 2009. Exposure of treating physician to radiation
 during prostate brachytherapy using iodine-125 seeds; dose measurements on both hands with
 thermoluminescence dosimeters. Strahlenther Onkol. 185(10):689-695.
- Schlattl, H., Zankl, M., Eder, H., et al., 2007. Shielding properties of lead-free protective clothing and
 their impact on radiation doses. Med. Phys. 34, 4270.
- Schueler, B.A., Vrieze, T.J., Bjarnason, H., et al., 2006. An investigation of operator exposure in interventional radiology. Radiographics 26, 1533–1541.
- Schultz, F.W., Zoetelief, J., 2006. Estimation effective dose for a cardiac catheterisation procedure with
 single and double dooimetry. Radiat. Prot. Dosim. 118, 196–204.
- Schultz, F.W., Zoetelief, J., 2008. Dosimeter readings and effective dose to the cardiologist with
 protective clothing in a simulated interventional procedure. Rad. Prot. Dosim. 129, 311–315.
- Schwartz, D.J., Davis, B.J., Vetter, R.J., et al., 2003. Radiation exposure to operating room personnel
 during transperineal interstitial permanent prostate brachytherapy. Brachytherapy. 2(2):98-102.
- Seierstad, T., Stranden, E., Bjering, K., et al., 2006. Doses to nuclear technicians in a dedicated PET/CT
 centre utilizing 18F fluorodeoxyglucose (FDG). Radiat. Prot. Dosim. 123, 243–249.
- Shatila, O.H., 2015. Occupational Radiation Dose during the Trans-Catheter Aortic Valve Replacement
 Procedure. Thesis for the Degree of Master of Science.Colorado State University. Available at
 https://www.google.es/#q=Shatila%2C+O.H.%2C+2015.+Occupational+Radiation+Dose+during+
 the+Trans-
- 2289 Catheter+Aortic+Valve+Replacement+Procedure.+Thesis+for+the+Degree+of+Master+of+Scienc 2290 e.+Colorado+State+University.
- Shortt, C.P., Al-Hashimi, H., Malone, L., et al., 2007. Staff radiation doses to the lower extremities in
 interventional radiology. Cardiovasc. Interv. Radiol. 30, 1206–1209.
- Siiskonen, T., Tapiovaara, M., Kosunen, A., et al., 2007. Monte Carlo simulations of occupational
 radiation doses in interventional radiology. Brit. J. Radiol. 80, 460–468.
- Siiskonen, T., Tapiovaara, M., Kosunen, A., et al., 2008. Occupational radiation doses in interventional
 radiology: simulations. Rad. Prot. Dosim. 129, 36–38.
- 2297 Sinclair, W.K., 1952. Artificial radioactive sources for interstitial therapy. Brit J Radiol. 25:417.
- SIRTEX Medical., 2016. SIR-Spheres (yttrium-90 resin microspheres) [package insert]. Available at:
 http://www.sirtex.com/media/34874/pi-ec-11.pdfAccessed Sept 1, 2016.



- Smathers, S., Wallner, K., Korssjoen, T., et al., 1999. Radiation safety parameters following prostate
 brachytherapy. Int J Radiat Oncol Biol Phys. 45(2):397-9.
- Smilowitz, N.R., Balter, S., Weisz, G., 2013. Occupational hazards of interventional cardiology.
 Cardiovasc. Revasc. Med. 14. 223–228.
- Srinivas, Y., Wilson, D.L., 2002. Image quality evaluation of flat panel and image intensifier digital
 magnification in x-ray fluoroscopy. Med. Phys. 29, 1611–1621.
- Stone, N.N., Stock, R.G., 2002. Permant seed implantation for localized adenocarcinoma of the prostate.
 Curr Urol Rep. 3(3):201-6.
- Stranden, E., Widmark, A., Sekse, T., 2008. Assessing doses to interventional radiologists using a
 personal dosimeter worn over a protective apron. Acta Radiol. 49, 415–418.
- Struelens, L., Schoonjans, W., Schils, F., et al., 2013. Extremity and eye lens dosimetry for medical
 staff performing vertebraplasty and kyphoplasty procedures. J. Radiol. Prot. 33, 635–645.
- Swiss Ordinance, 2008. Eidgenössisches Departement des Inneren und Eidgenössisches Departement
 für Umwelt, Verkehr, Energie und Kommunikation: Verordhung über die Personendosimetrie
 (Dosimetrieverordnung) vom 07.10.1999 (Vers. 1 January 2008); SR 814.501.43. Bern; 2008 (in
 German).
- Teeuwisse, W.M., Geleijns, J., Broerse, J.J., et al., 2001. Patient and staff dose during CT guided biopsy,
 drainage and coagulation. Br. J. Radiol. 74, 720–726.
- Theocharopoulos, N., Damilakis, J., Perisinakis, K., et al., 2006. Occupational exposure in the
 electrophysiology laboratory quantifying and minimising radiation burden. Brit. J. Radiol. 79, 644–
 651.
- Thomadsen, B.R., Biggs, P.J., Cardarelli, G.A., et. al., 2020. Electronic intracavitary brachytherapy
 quality management based on risk analysis: The report of AAPM TG 182. Med. Phys. 47, e65 e91.
 DOI 0094-2405/2020/47(4)/e65/27.
- Thomadsen, B.R., Lin S-W., Laemmrich P., et al., 2003. Analysisof treatment delivery errors in
 brachytherapy using formal risk analysis techniques. Int. J. Radiat. Oncol. Biol. Phys. 57, 1492 –
 1508.
- Thomadsen, B.R., Rivard, M., Butler, W.M. (eds), 2005. *Brachytherapy Physics*, 2nd edition. Medical
 Physics Publishing : Madison.
- Thornton, R.H., Dauer, L.T., Altamirano, J.P., et al., 2010. Comparing strategies for operator eye
 protection in the interventional radiology suite. J. Vasc. Interv. Radiol.21, 1703–1707.
- Tosi, G., 2003, Report on one accident occurred in a nuclear medicine department in Italy, 6th European
 ALARA Network Workshop. Madrid, 2002; ISBN: 84-7834-437-3. Proceedings edited by CIEMAT,
 Madrid 2003.
- Trout, E.D., 1977. Isodose curves in a phantom due to diagnostic quality X-radiation. Health Phys. 33,
 359–367.
- Trumm, C.G., Pahl, A., Helmberger, T.K., et al., 2012. CT fluoroscopy-guided percutaneous
 vertebroplasty in spinal malignancy: technical results, PMMA leakages, and complications in 202
 patients. Skeletal Radiol. 41, 1391–1400.
- Tsapaki, V., Kottou, S., Vañó, E., et al., 2004. Occupational dose constraints in interventional cardiology procedures: the DIMOND approach. Phys. Med. Biol. 49, 997–1005.
- Uthoff, H., Peña, C., West, J., et al., 2013. Evaluation of novel disposable, light-weight radiation
 protection devices in an interventional radiology setting: a randomized controlled trial. AJR Am J
 Roentgenol. 200. 915–920.
- Uzoigwe, C.E., Middleton, R.G., 2012. Occupational radiation exposure and pregnancy in orthopaedics.
 J. Bone Joint Surg. Br. 94, 23–27.
- Vaidya, J.S., Wenz, F., Bulsara, M., et al., 2014. Risk-adapted targeted intraoperative radiotherapy
 versus whole-breast radiotherapy for breast cancer: 5-year results for local control and overall
 suvival from the TARGIT-A randomizsed trial. Lancet 383:603-613.
- Van Haaren, P.M., van't Riet, A., Moerland, M.A., et al., 2011. Dose to fingertips of staff preparing
 stranded iodine-125 seeds for permanent prostate implants. Radiat Prot Dosim. 145(1):61-65.



- Van Rooijen, B.D., de Haan, M.W., Das, M., et al., 2014. Efficacy of radiation safety glasses in interventional radiology. Cardiovasc. Intervent. Radiol. 37, 1149–1155.
- Vanhavere, F., Carinon, E., Gualdrini, G., et al., 2012. ORAMED: Optimisation of Radiation Protection
 for Medical Staff. 7th EURADOS Report 2012.
- Vanhavere, F., Covens, P., 2010. Testing the direct ion storage dosimeter for personal dosimetry in a
 nuclear research centre and a hospital. Radiat. Prot. Dosim. 138, 334–339.
- Vañó, E., González, L., Beneytez, F., et al., 1998. Lens injuries induced by occupational exposure in
 non-optimised interventional radiology laboratories. Br. J. Radiol. 71, 728–733.
- Vaño, E., Gonzalez, L., Fernandez, J.M., et al., 2006. Occupational radiation doses in interventional cardiology: a 15-year follow-up. Br. J. Radiol. 79, 383–388.
- Vañó, E, Gonzalez, L., Fernandez, J.M., et al., 2008a. Eye lens exposure to radiation in interventional
 suites: caution is warranted. Radiology 248, 945–953.
- Vañó, E., Järvinen, H., Kosunen, A., et al., 2008b. Patient dose in interventional radiology: a European
 survey. Radiat. Prot. Dosim. 129, 39–45.
- Vañó, E., Kleiman, N.J., Duran, A., et al., 2010. Radiation cataract risk in interventional cardiology
 personnel. Radiat. Res. 174, 490–495.
- Vañó, E., Kleiman, N.J., Duran, A., et al., 2013a. Radiation-associated lens opacities in catheterization
 personnel: results of a survey and direct assessments. J. Vasc. Interv.Radiol. 24, 197–204.
- Vañó, E., Fernández, J.M., Sánchez, R.M., et al., 2013b. Realistic approach to estimate lens doses and
 cataract radiation risk in cardiology when personal dosimeters have not been regularly used. Health
 Phys.105, 330-339.
- Vañó, E., 2015a. Occupational radiation protection of health workers in imaging. Radiat. Prot. Dosim.
 164, 126–129.
- Vañó, E., Sanchez, R.M., Fernandez, J.M., et al., 2015b. A set of patient and staff dose data for
 validation of Monte Carlo calculations in interventional cardiology. Radiat. Prot. Dosim. 165, 235–
 239.
- Vañó, E., Sanchez, R.M., Fernandez, J.M., 2015c. Estimation of staff lens doses during interventional
 procedures. Comparing cardiology, neuroradiology and interventional radiology. Radiat. Prot.
 Dosime. 165, 279–283.
- Vano, E., Fernandez, J.M., Resel, L.E., et al., 2016. Staff lens doses in interventional urology. A
 comparison with interventional radiology, cardiology and vascular surgery values. J. Radiol. Prot.
 36, 37–48.
- Vañó, E., Personal communication, 2016. (see also IAEA training material https://rpop.iaea.org/RPOP/RPoP/Content/AdditionalResources/Training/1_TrainingMaterial/NonradiologistsNon-cardiologists.htm).
- Venkatesan, A., Kadoury, S., Abi-Jaoudeh N., et al., 2011. Real-time FDG PET guidance during
 biopsies and radiofrequency ablation using multimodality fusion with electromagnetic navigation.
 Radiology 260, 848–856.
- Venselaar, J.M., Peréz-Calatayud, J. (Eds.), 2004. A practical guide to quality control of brachytherapy
 equipment. ESTRO: Brussels.
- Von Boetticher, H., Lachmund, J., Hoffmann, W., 2010. An analytic approach to double dosimetry
 algorithms in occupational dosimetry using energy dependent organ dose conversion coefficients.
 Health Phys. 99, 800–805.
- Wakabayashi, M., Osawa, T., Mitsuhashi, H., et al., 1971. High dose rate intracavitary using the
 RALSTRON. Nippon Acta Radiol 31:340-378, 1971.
- 2396 Wagner, L.K., Hayman, L.A., 1982. Pregnancy and women radiologists. Radiology, Volume: 145:2.
- Wagner, L.K., Mulhern, O.R., 1996. Radiation-attenuating surgical gloves: effects of scatter and
 secondary electron production. Radiology 200, 45–48.
- Wagner, L.K., Archer, B.R., 2004. Minimizing Risks from Fluoroscopic x- rays: Bioeffects,
 Instrumentation and Examination (4th ed.). Partners in Radiation Management Woodlands, TX.
- Wenzl, T.B., 2005. Increased brain cancer risk in physicians with high radiation exposure. (letter)
 Radiology. 235. 709–710.



- Werner, M.K., Aschoff, P., Reimold, M., et al., 2011. FDG-PET/CT-guided biopsy of bone metastases
 sets a new course in patient management after extensive imaging and multiple futile biopsies. Br. J.
 Radiol. 84, e65–67.
- Wernli, C., Kahilainen, J., 2001. Direct ion storage dosimetry systems for photon, beta and neutron
 radiation with instant readout capabilities. Radiat. Prot. Dosim. 96, 255–259.
- Whitby, M., Martin, C.J., 2003. Radiation doses to the legs of radiologists performing interventional
 procedures: are they a cause for concern? Brit. J. Radiol. 76, 321–327.
- Whitby, M., Martin, C.J., 2005. A study of the distribution of dose across the hands of interventional
 radiologists and cardiologists. Brit. J. Radiol. 78, 219–229.
- White, S., Binns, D., Johnston, V.V., et al., 2000. Occupational exposure in nuclear medicine and PET.
 Clin. Positron Imaging 3, 127–129.
- WHO, 2000. Efficacy and radiation safety in interventional radiology. World Health Organization,
 Geneva.
- Williamson, M., Dauer, L., 2014. Activity thresholds for patient instruction and release for positron
 emission tomography radionuclides. Health Phys. 106, 341–352.
- 2418 Yoder, C., Salasky, M., 2016. A review of the use of two methods practiced in the United States to
- assess the effective dose equivalent for fluoroscopic-based radiology. Radiat. Prot. Dosim. 170, 307–
- 2420 310.



GLOSSARY

2422 Absorbed dose (D)

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2425

The quotient of the mean energy, imparted to an element of matter by ionising radiation and the mass of the element.

$$D = \frac{\mathrm{d}\overline{\varepsilon}}{\mathrm{d}m}$$

2426Absorbed dose is the basic physical dose quantity and is applicable to all types of ionising2427radiation and to any material. Absorbed dose is a measurable quantity for which primary2428standards exist. In the International System of Units, SI, the unit for absorbed dose is the ratio2429J(joule)/kg(kilogramme) to which the special name of gray (Gy) is given.

2430 Acceptance test

2431A test carried out after new equipment has been installed or major modifications have been2432made to existing equipment, in order to verify compliance with the manufacturer's2433specifications, contractual specifications and applicable local regulations or equipment2434standards.

2435 ALARA

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An acronym for As Low As Reasonably Achievable. See Optimisation of protection.

2437 Becquerel (Bq)

The special name for the SI unit of activity. 1 Bq = 1 s⁻¹ ($\approx 2.7 \times 10^{-11}$ Ci).

- 2439 Brachytherapy
- Radiation treatment technique that utilises radioactive sources inserted directly into tumours, cavities, vessels, or simply placed in contact with a target tissue.
- 2442 Carers and comforters
- Individuals, other than staff, who care for and comfort patients. These individuals include
 parents and others, normally family or close friends, who hold children during diagnostic
 procedures or may come close to patients following the administration of radiopharmaceuticals
 or during brachytherapy (ICRP, 2007).
- 2447ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological2448Protection. ICRP Publication 103. Ann. ICRP 37(2-4).
- 2449 Commissioning
- Testing carried out after new equipment has been installed, in order to verify that the equipment is properly configured for its clinical application at the centre (NCRP, 2010).
- 2452NCRP, 2010. Radiation dose management for fluoroscopically guided interventional2453medical procedures. NCRP Report No. 168. National Council on Radiation Protection2454and Measurements, Bethesda, MD.
- 2455 Constancy test
- Each of a series of tests, carried out to ensure that the functional performance of equipment meets established criteria, or to enable the early recognition of changes in the properties of components of the equipment (IEC, 1993).



2459 2460 2461	IEC, 1993. Medical electrical equipment - Part 1-61223: Evaluation and routine 726 testing in medical imaging departments. 1st ed. Geneva, Switzerland: 727 International Electrotechnical Commission.		
2462	Deterministic effect		
2463	See Tissue reaction.		
2464	Dose coefficient		
2465 2466 2467 2468	Used to express dose per unit intake of a radioactive substance, but sometimes also used to describe other coefficients linking quantities or concentrations of activity to doses or dose rates, such as the external dose rate at a specified distance above a surface with a deposit of a specified activity per unit area of a specified radionuclide (ICRP, 2007).		
2469 2470	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2471	Dose limit		
2472 2473	The value of the effective dose or the equivalent dose to individuals from planned exposure situations that shall not be exceeded (ICRP, 2007).		
2474 2475	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2476	Dosimeter over apron		
2477	Dosimeter unshielded by the protective apron.		
2478	Dosimeter under apron		
2479	Dosimeter shielded by the protective apron		
2480	Effective dose (E)		
2481 2482	The tissue-weighted sum of the equivalent doses in all specified tissues and organs of the body, given by the expression:		
2492	$E = \sum_{\mathrm{T}} w_{\mathrm{T}} H_{\mathrm{T}} = \sum_{\mathrm{T}} w_{\mathrm{T}} \sum_{\mathrm{R}} w_{\mathrm{R}} D_{\mathrm{T,R}}$		
2483	where w_{τ} is the tissue weighting factor for tissue or organ T and w_{τ} is the radiation weighting		
2485 2486	factor. The unit for the effective dose is the same as for absorbed dose, $J \text{ kg}^{-1}$, and its special name is sievert (Sv).		
2487 2488 2489	The sum is performed over all organs and tissues of the human body considered to be sensitive to the induction of stochastic effects. The tissue weighting factors are age- and sex-averaged, and intended to apply as rounded values to a population of both sexes and all ages.		
2490	Employer		
2491 2492 2493 2494 2495	An organisation, corporation, partnership, firm, association, trust, estate, public or private institution, group, political or administrative entity, or other persons designated in accordance with national legislation, with recognised responsibility, commitment, and duties towards a worker in her or his employment by virtue of a mutually agreed relationship. A self-employed person is regarded as being both an employer and a worker (ICRP, 2007).		
2496 2497	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2498	Equivalent dose (H _T)		



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2500

The dose in a tissue or organ T given by:

$$H_{\rm T} = \sum_{\rm R} w_{\rm R} D_{\rm T,R}$$

2501 where $D_{T,R}$ is the mean absorbed dose from radiation R in a tissue or organ T, and w_R is the 2502 radiation weighting factor. Since w_R is dimensionless, the unit for the equivalent dose is the 2503 same as for absorbed dose, J kg⁻¹, and its special name is sievert (Sv).

2504 Fluoroscopically or CT guided interventions

Procedures comprising guided therapeutic and diagnostic interventions, by percutaneous or other access, usually performed under local anaesthesia and/or sedation, with fluoroscopic or CT imaging used to localise the lesion/treatment site, monitor the procedure, and control and document the therapy (ICRP, 2000). 3D (Cone Beam CT) imaging using fluoroscopic equipment is also used in some interventional procedures.

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ICRP, 2000. Avoidance of radiation injuries from medical interventional procedures. ICRP Publication 85. Ann. ICRP 30(2).

2512 Gray (Gy)

2513 The special name for the SI unit of absorbed dose: $1 \text{ Gy} = 1 \text{ J kg}^{-1}$.

2514 Justification

The process of determining whether either (1) a planned activity involving radiation is, overall, beneficial [i.e. benefits to individuals and to society from introducing or continuing the activity outweigh the harm (including radiation detriment) resulting from the activity]; or (2) a proposed protection strategy in an emergency or existing exposure situation is likely, overall, to be beneficial [i.e., whether the benefits to individuals and to society (including the reduction in radiation detriment) from introducing or continuing the protection strategy outweigh its cost and any harm or damage it causes] (ICRP, 2007).

- 2522ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological2523Protection. ICRP Publication 103. Ann. ICRP 37(2-4).
- 2524 Mean absorbed dose in a tissue or organ (T) $(D_{\rm T})$
- 2525 The absorbed dose $D_{\rm T}$, averaged over the tissue or organ T, which is given by:

 $D_{\mathrm{T}} = rac{\varepsilon_{\mathrm{T}}}{m_{\mathrm{T}}}$

- 2526
- 2527 where $\varepsilon_{\rm T}$ is the mean total energy imparted in a tissue or organ T, and $m_{\rm T}$ is the mass of that 2528 tissue or organ (ICRP, 2007).
- 2529ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological2530Protection. ICRP Publication 103. Ann. ICRP 37(2-4).
- 2531 Medical exposure
- Exposure incurred by patients as part of their own medical or dental diagnosis or treatment; by persons, other than those occupationally exposed, knowingly, while voluntarily helping in the support and comfort of patients; and by volunteers in a programme of biomedical research involving their exposure (ICRP, 2007).
- 2536ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological2537Protection. ICRP Publication 103. Ann. ICRP 37(2-4).



2538 Occupational exposure

2539	This refers to all exposures incurred by workers in the course of their work, with the exception
2540	of 1) excluded exposures and exposures from exempt activities involving radiation or exempt
2541	sources; 2) any medical exposure; and 3) the normal local natural background radiation.
2542	However, because of the ubiquity of radiation, the Commission therefore limits its use of
2543	'occupational exposures' to radiation exposures incurred at work as a result of situations that
2544	can reasonably be regarded as being the responsibility of the operating management. Excluded
2545	exposures and exposures from exempt practices or exempt sources generally do not need to be
2546	accounted for in occupational protection (ICRP, 2007).

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ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).

2549 Operational quantities

Quantities used in practical applications for monitoring and investigating situations involving external exposure. They are defined for measurements and assessment of doses in the body. In internal dosimetry, no operational dose quantities have been defined which directly provide an assessment of equivalent or effective dose. Different methods are applied to assess the equivalent or effective dose due to radionuclides in the human body. They are mostly based on various activity measurements and the application of biokinetic models (computational models).

- 2557 Optimisation of protection (and safety)
- The process of determining what level of protection and safety makes exposures, and the probability and magnitude of potential exposures, as low as reasonably achievable, economic and societal factors being taken into account (ICRP, 2007). In medical imaging and radiotherapy procedures, optimisation of radiological protection means keeping the doses 'as low as reasonably achievable, economic and societal factors being taken into account', and is best described as management of the radiation dose to the patient to be commensurate with the medical purpose.
- 2565

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ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).

2567 Personal dose equivalent

2568 The operational quantity for individual monitoring is the personal dose equivalent Hp(d) which is the dose equivalent in soft tissue at an appropriate depth, d in mm, below a specific point on 2569 the human body. The unit of personal dose equivalent is joule per kilogram (J kg⁻¹) and its 2570 special name is sievert (Sv). The specified point is usually given by the position where the 2571 individual's dosimeter is worn. For monitoring the effective dose the operational quantity 2572 Hp(10), and for the assessment of the dose to the skin and to the hands and feet the personal 2573 2574 dose equivalent, Hp(0.07) is used. A depth d=3 mm is adequate for monitoring the dose to the lens of the eye. In practice, however, in many countries, calibration of dosimeters in terms 2575 Hp(3) has not been implemented, but Hp(0.07) can be used for the same monitoring purpose 2576 for photon radiation, which is the case in interventions guided by radiological imaging. 2577

2578 Principles of protection

A set of principles that apply to radiation sources and to the individual in controllable exposure situations. The principle of justification and the principle of optimisation of protection are source related and apply in all exposure situations. The principle of application of dose limits is individual related and only applies in planned exposure situations (ICRP, 2007).



2583 2584	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2585	Radiation weighting factor (w_R)		
2586 2587 2588 2589	A dimensionless factor by which the organ or tissue absorbed dose is multiplied to reflect the higher biological effectiveness of high-linear energy transfer (LET) radiations compared with low-LET radiations. It is used to derive the equivalent dose from the absorbed dose averaged over a tissue or organ (ICRP, 2007).		
2590 2591	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2592	Sievert (Sv)		
2593 2594	The special name for the SI unit of equivalent dose, effective dose, and operational dose quantities. The unit is joule per kilogram (J kg ^{-1}).		
2595	Staff		
2596 2597 2598 2599	In the context of this document, staff are healthcare workers (see Workers) who participate in the care of a patient during a radiological procedure (e.g. physicians, nurses, radiographers) or who may be exposed to radiation from medical imaging equipment during the course of their work (e.g. equipment service personnel, janitorial staff).		
2600	Stenosis		
2601 2602	Narrowing of a hollow structure. With respect to coronary artery anatomy, this refers to narrowing of the inner diameter of a coronary artery.		
2603	Stochastic effects of radiation		
2604 2605	Malignant disease and heritable effects for which the probability of an effect occurring, but not its severity, is regarded as a function of dose without threshold.		
2606	Threshold dose for tissue reactions		
2607	Dose estimated to result in 1% incidence of tissue reactions (ICRP, 2007).		
2608 2609	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2610	Tissue reaction		
2611 2612 2613 2614	Injury in populations of cells, characterised by a threshold dose and an increase in the severity of the reaction as the dose is increased further. Tissue reactions are also termed 'deterministic effects'. In some cases, tissue reactions are modifiable by postirradiation procedures including biological response modifiers (ICRP, 2007).		
2615 2616	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological Protection. ICRP Publication 103. Ann. ICRP 37(2-4).		
2617	Tissue weighting factor (<i>w</i> _T)		
2618 2619 2620	A factor by which the equivalent dose in a tissue or organ T is weighted to represent the relative contribution of that tissue or organ to the total health detriment resulting from uniform irradiation of the body (ICRP, 1991). It is weighted (ICRP, 2007) such that:		

$$\sum_{\rm T} w_{\rm T} = 1$$



2622	ICRP, 1991. 1990 Recommendations of the International Commission on Radiological
2623	Protection. ICRP Publication 60. Ann. ICRP 21(1-3).
2624	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological
2625	Protection. ICRP Publication 103. Ann. ICRP 37(2-4).
2626	Worker
2627	Any person who is employed, whether full time, part time or temporarily, by an employer, and
2628	who has recognised rights and duties in relation to occupational radiological protection.
2629	Workers in medical professions involving radiation are occupationally exposed (ICRP, 2007).
2630	ICRP, 2007. The 2007 Recommendations of the International Commission on Radiological
2631	Protection. ICRP Publication 103. Ann. ICRP 37(2-4).
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